

BioMEMS and Nanoparticles for the Detection and Treatment of Cancer

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Background and Introduction

- Richard Feynmann – There's lots of room at the bottom....(1961 APS talk)
- Several people could benefit from implantable or injectable systems for class detection and treatment
- This talk examines two types of small structures for cancer detection

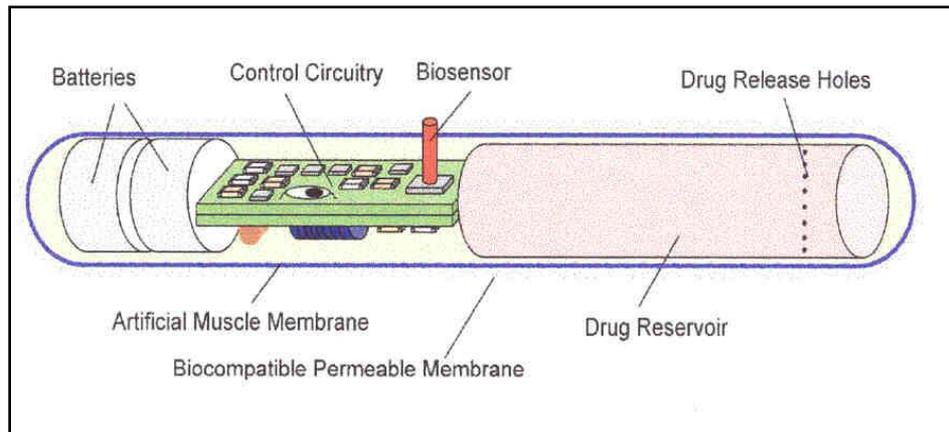
Why the Focus on Cancer?

- Several people suffer from cancer – either directly or through contact with someone that has cancer
- The biggest problem is really one of early detection – existing methods of detection are limited in spatial resolution
- The other major problem is the severe effect of existing cancer treatment methods e.g. radiation and chemotherapy (localized therapeutics to be addressed in the next class)
- This class presents some new ideas on cancer detection
 - BioMEMS for the detection of cancer
 - Magnetic nanoparticles for cancer detection

Introduction to BioMEMS Systems

- BioMEMS structures are micron-scale devices that are used in biomedical or biological applications
- At this scale, a wide range of devices are being made (e.g. pressure sensors, drug delivery systems, and cantilever detection systems)
- Explosive growth in emerging markets – civilian and military applications expected to reach multi-billion dollar levels

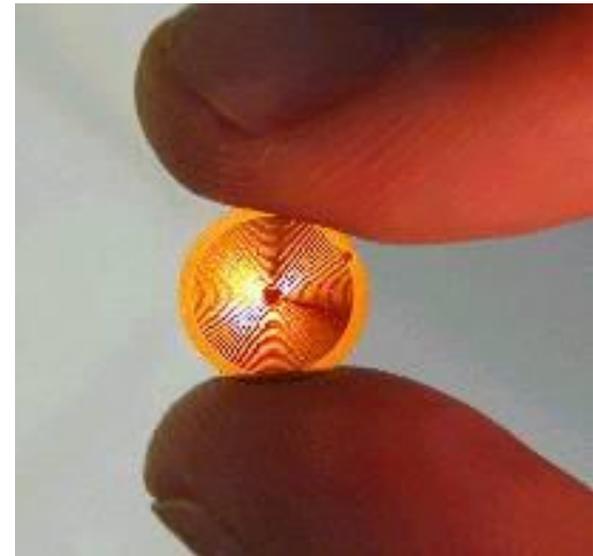
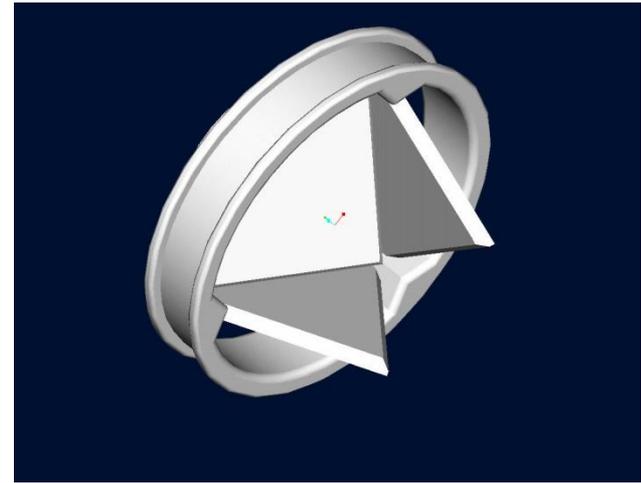
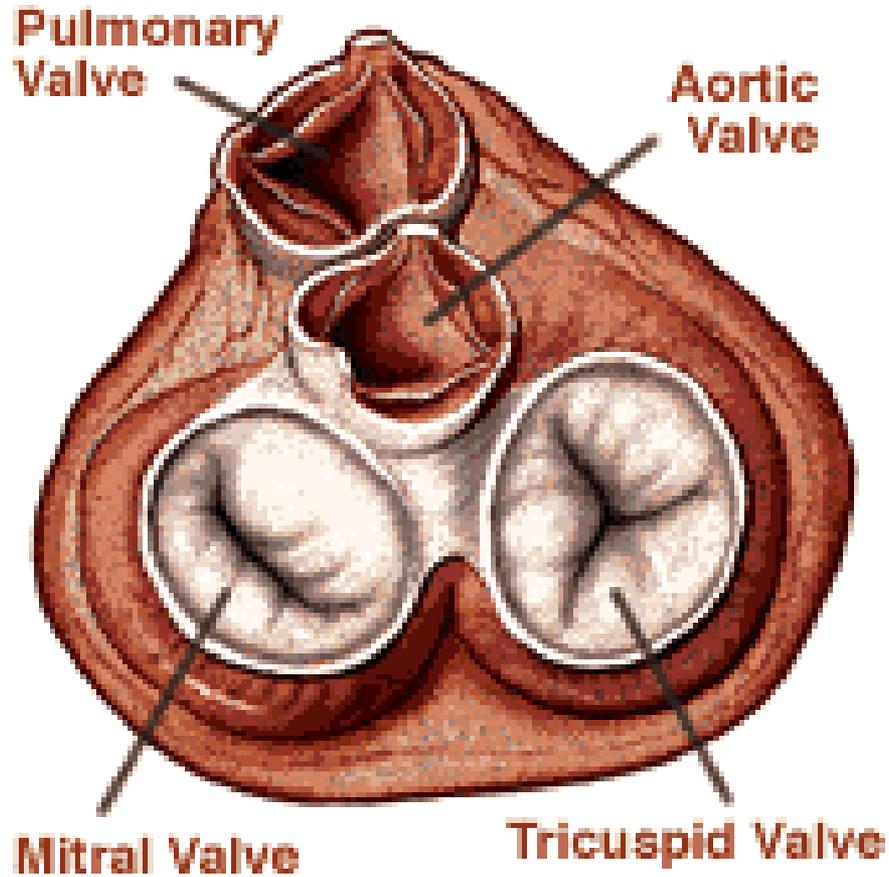
Drug Delivery System



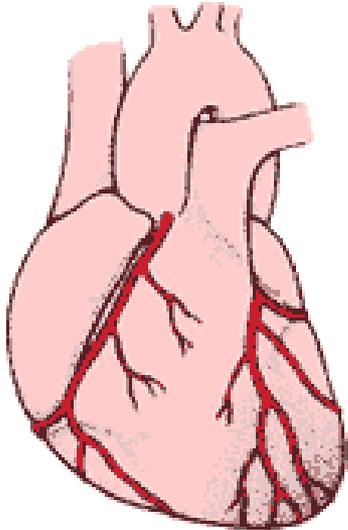
Implantable Blood Pressure Sensor



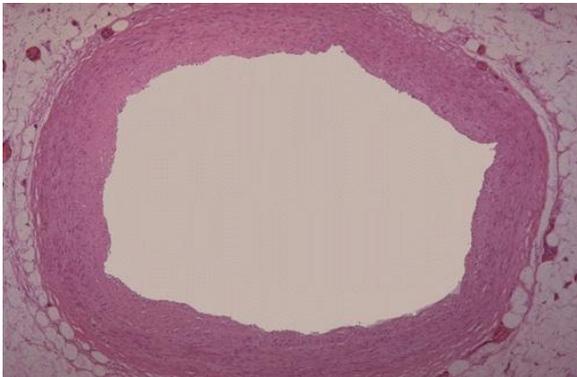
MEMS-Enhanced Trileaflet Valve



Atherosclerosis



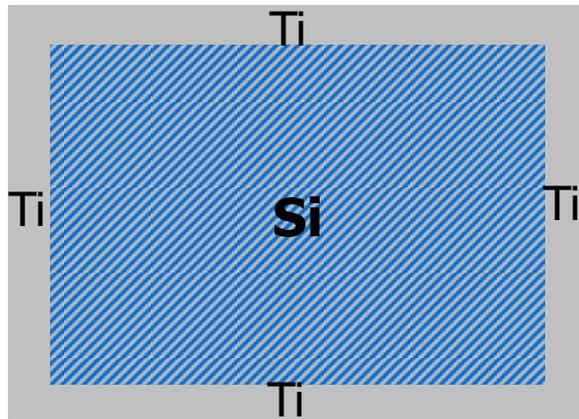
- Atherosclerosis is the hardening and narrowing of blood vessels caused by buildup of plaque
- Plaque is made up of cholesterol, calcium, and other blood components that stick to the vessel walls
- When plaque bursts, blood tends to clot, thus creating more blockage



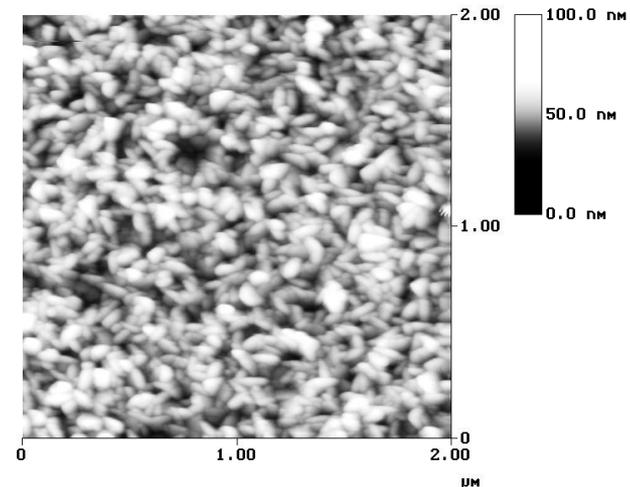
Biocompatibility of Silicon MEMS Systems

- Si is not the most biocompatible material
- Can be made biocompatible through the use of polymeric or Ti coatings.
- Polymeric coatings used on Si drug release systems.
- Ti coating approaches are also being developed.

Coated BioMEMS Structure



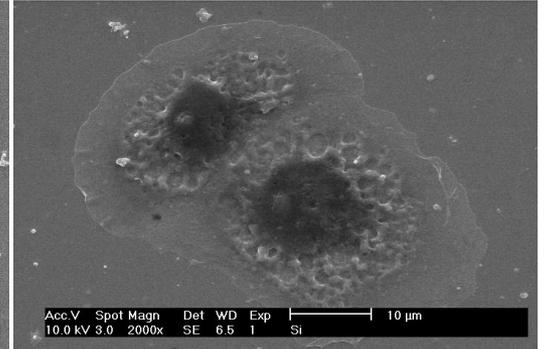
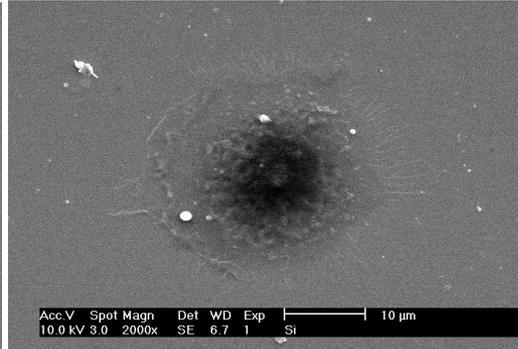
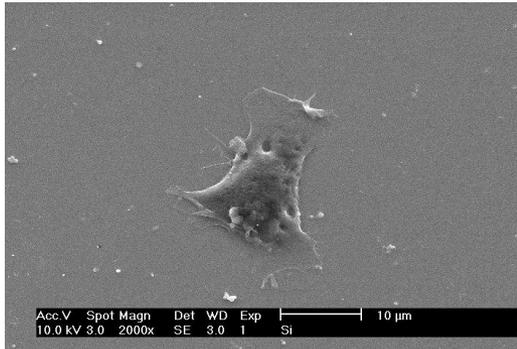
500 nm Ti Layer on Si



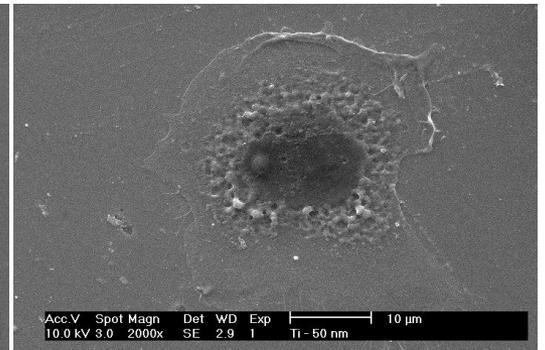
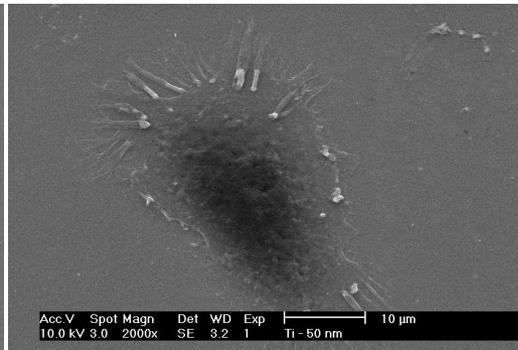
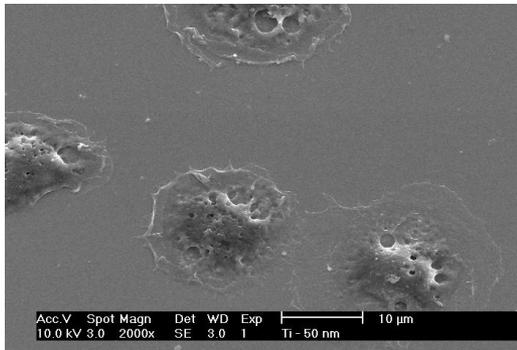
SURFACE CHEMISTRY – CELL SPREADING

HOS Cells

Si



Si - 50 nm
Titanium



30 minutes

60 minutes

120 minutes

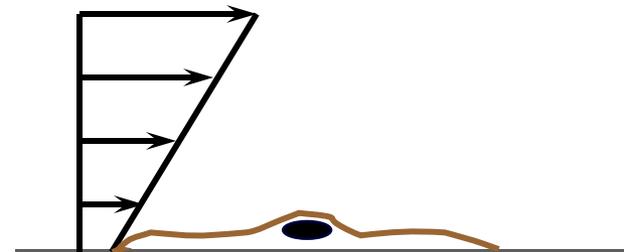
SHEAR ASSAY MEASUREMENT OF CELL ADHESION

- Shear stress for detachment is given by

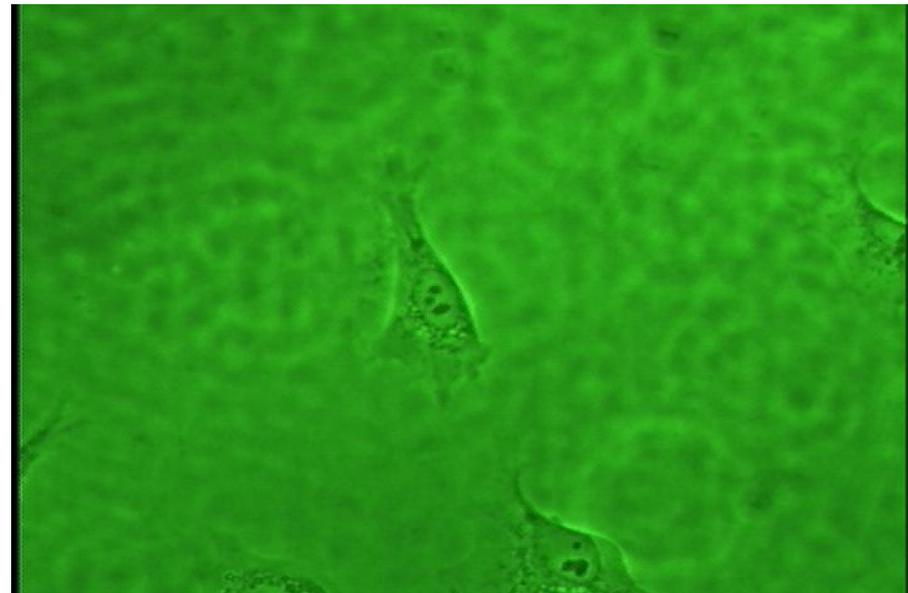
$$\tau = \frac{6Q\mu}{wh^2}$$

- Where Q - flow rate & μ -dynamic viscosity
- Considering initial onset of detachment to correspond to "adhesion" strength:
 - $\tau = 70$ Pa Polystyrene (PS)
 - $\tau = 81$ Pa Ti Coated PS

Shear Flow Schematic

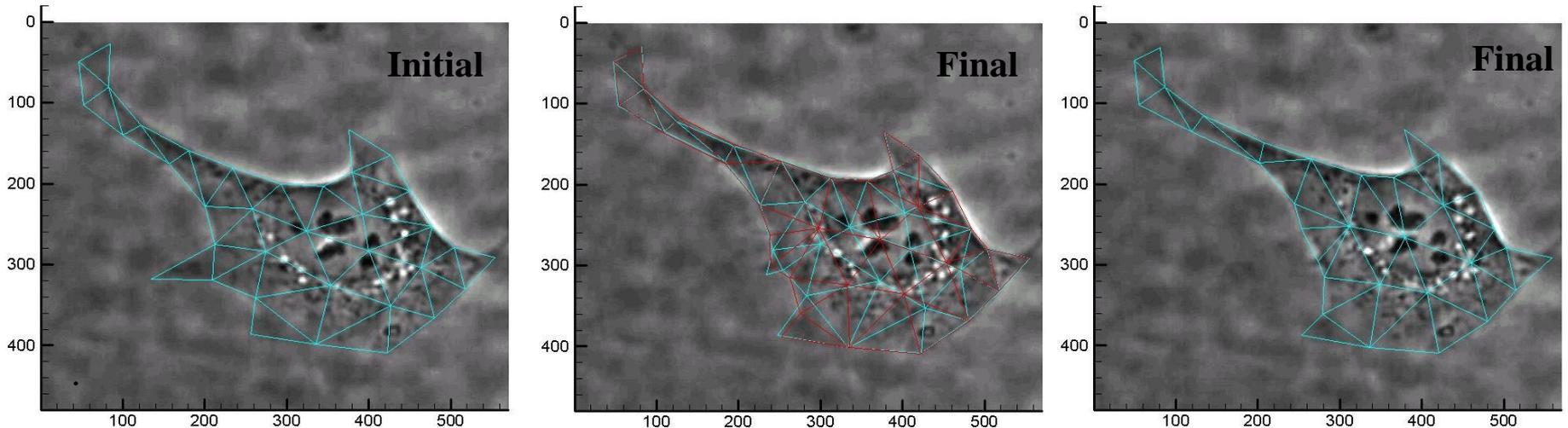


Cell Detachment

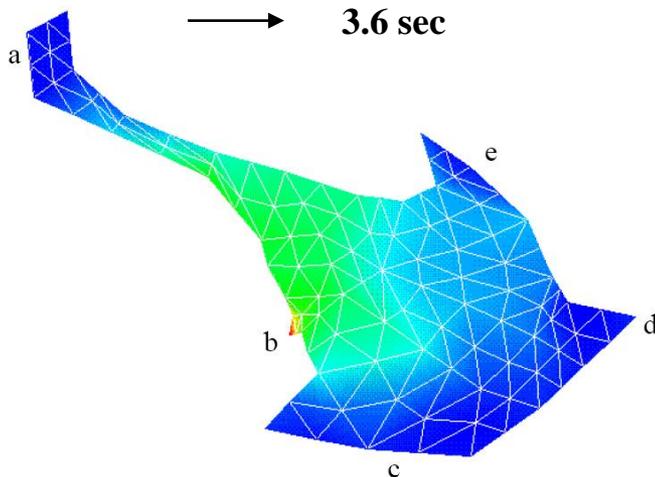
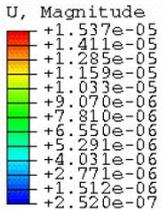
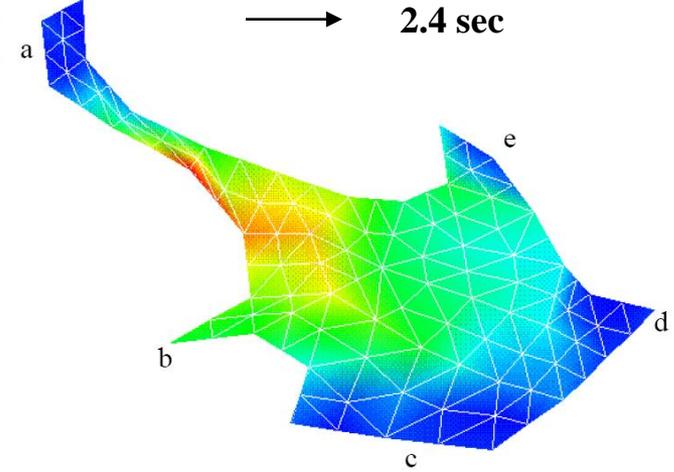
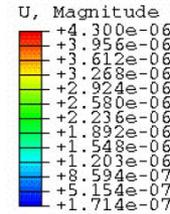
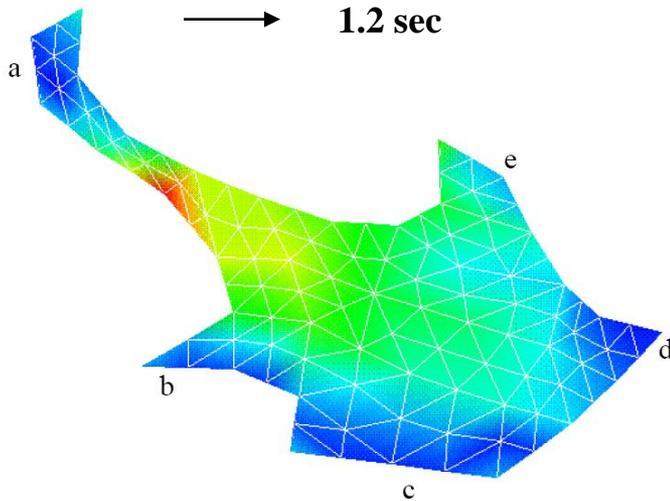
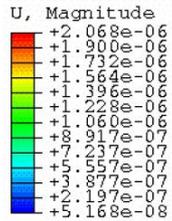


Digital Image Correlation

- Global Digital Image Correlation (GDIC) can be effectively utilized to characterize the cell deformation pattern by sequential correlating the images recorded during the assay shear test.
- The deformation mapping between these two images is obtained by a multi-variable minimization which conducted on a constrained system determined by the mesh
- Due to the severe deformations experienced by the cell during the assay test, a remeshing step is required to preserve the mesh quality



Cellular Displacement Subjected to Shear Flow

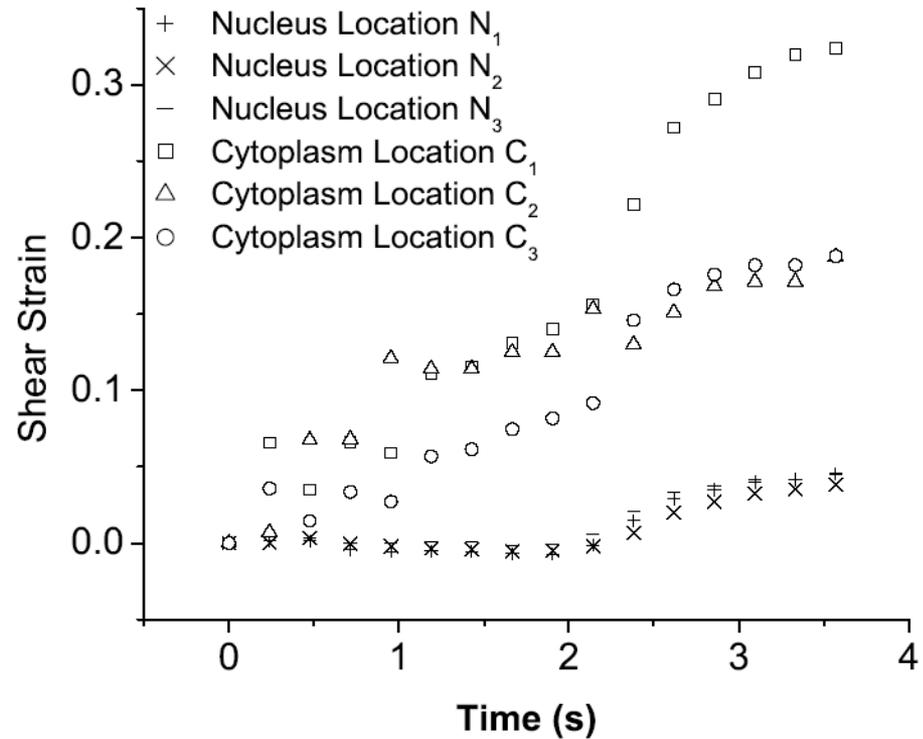
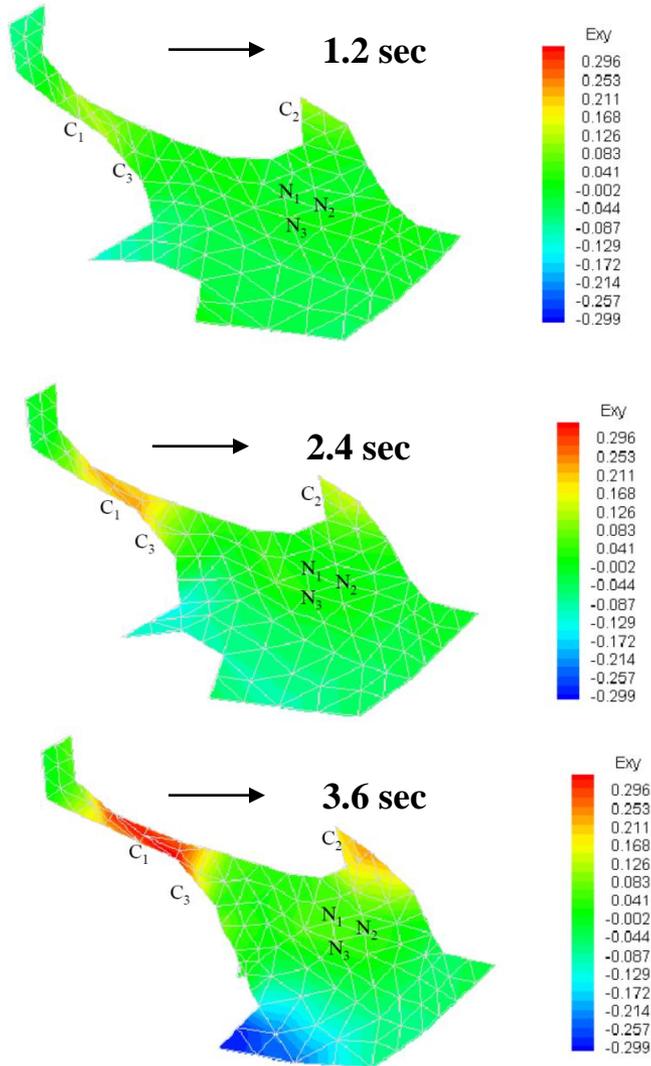


Higher mobility was observed at the rear edge (region b), compared to the front edge subjected to shear flow



displacement.avi

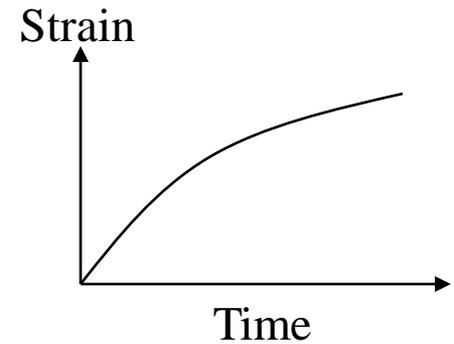
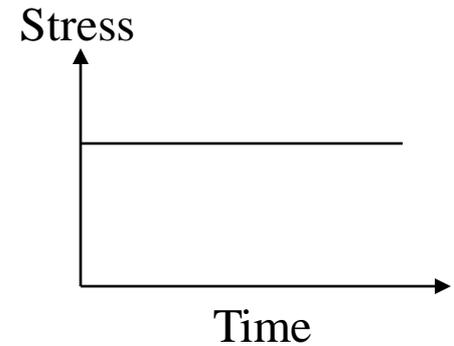
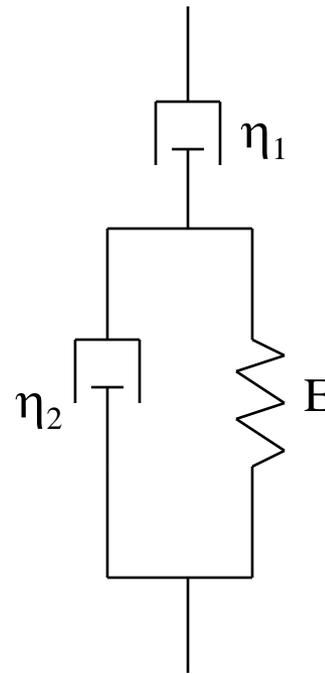
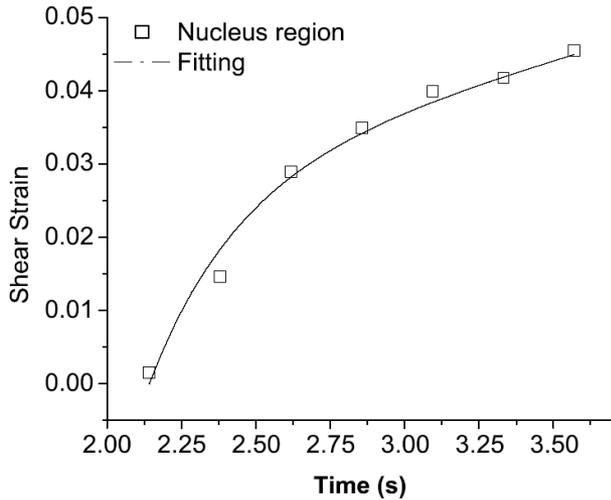
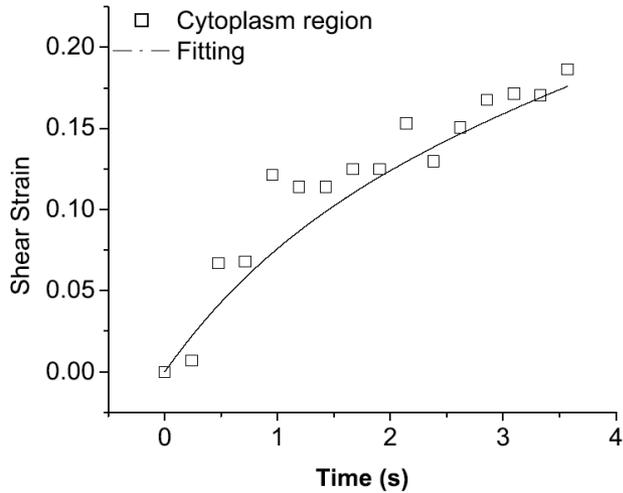
Cellular Strain Subjected to Shear Flow



The shear strains in cytoplasm increased more significantly than those obtained in the nucleus during the shear assay experiment

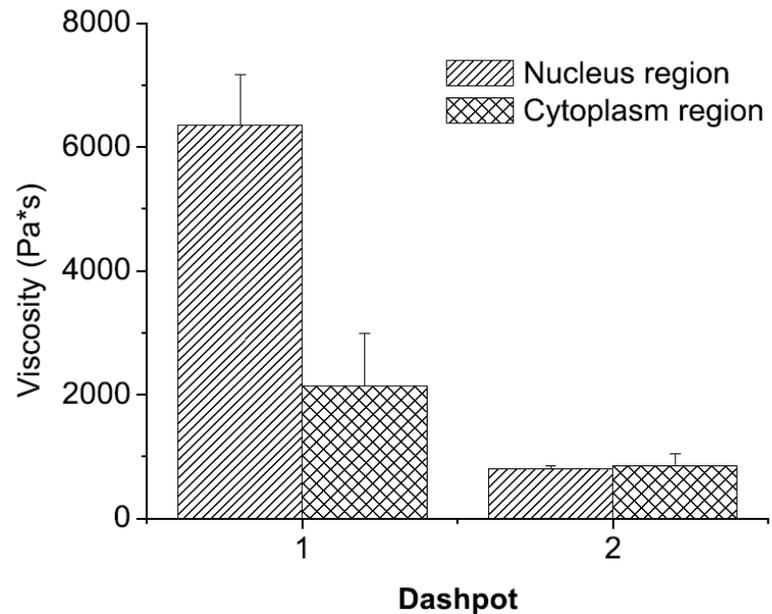
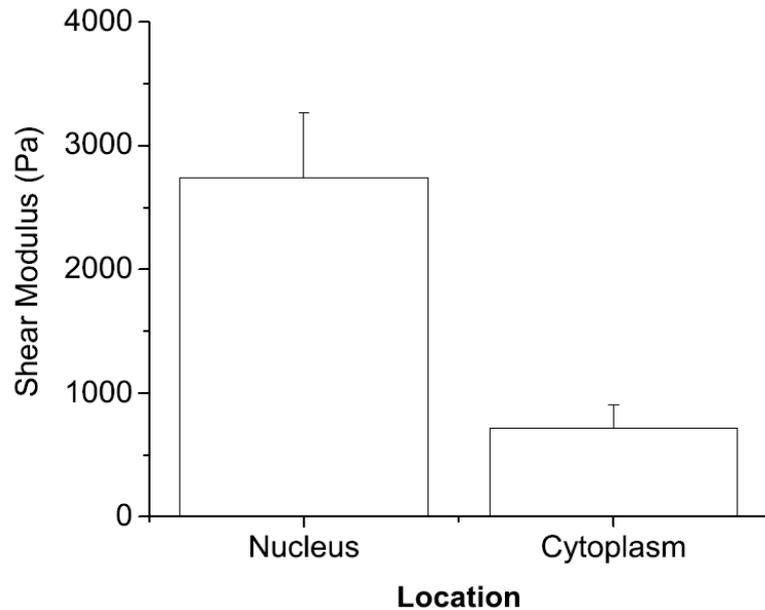


Viscoelastic Modeling



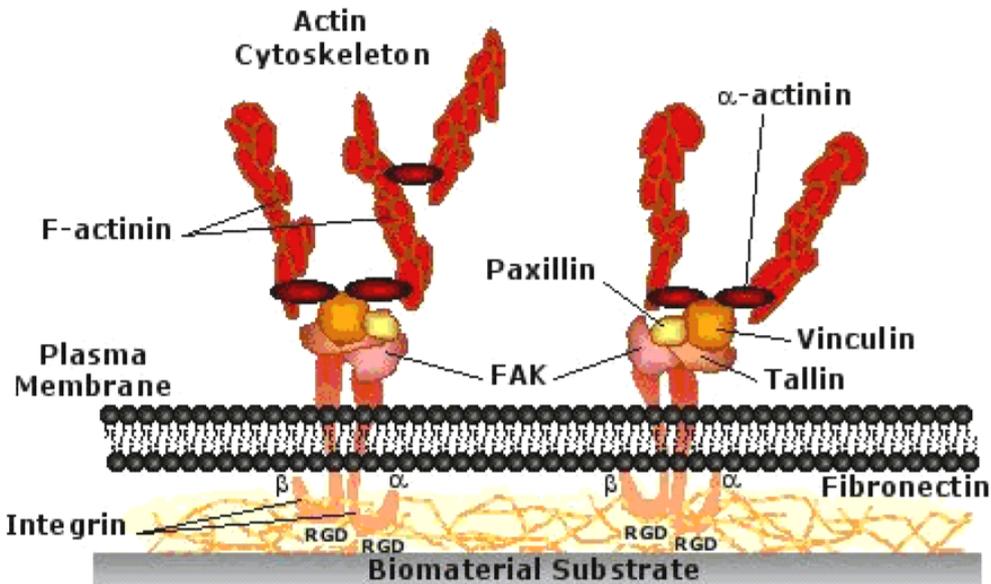
$$\epsilon = \frac{\sigma}{E} \left[1 - \exp\left(\frac{-t}{\tau}\right) \right] + \frac{\sigma}{\eta_1} t$$

Obtained Shear Moduli and Viscosities



The fact that the nucleus is more rigid than the cytoplasm can explain why the nucleus deforms less than the cells when subjected to shear flow in the current study, or when the substrate is stretched.

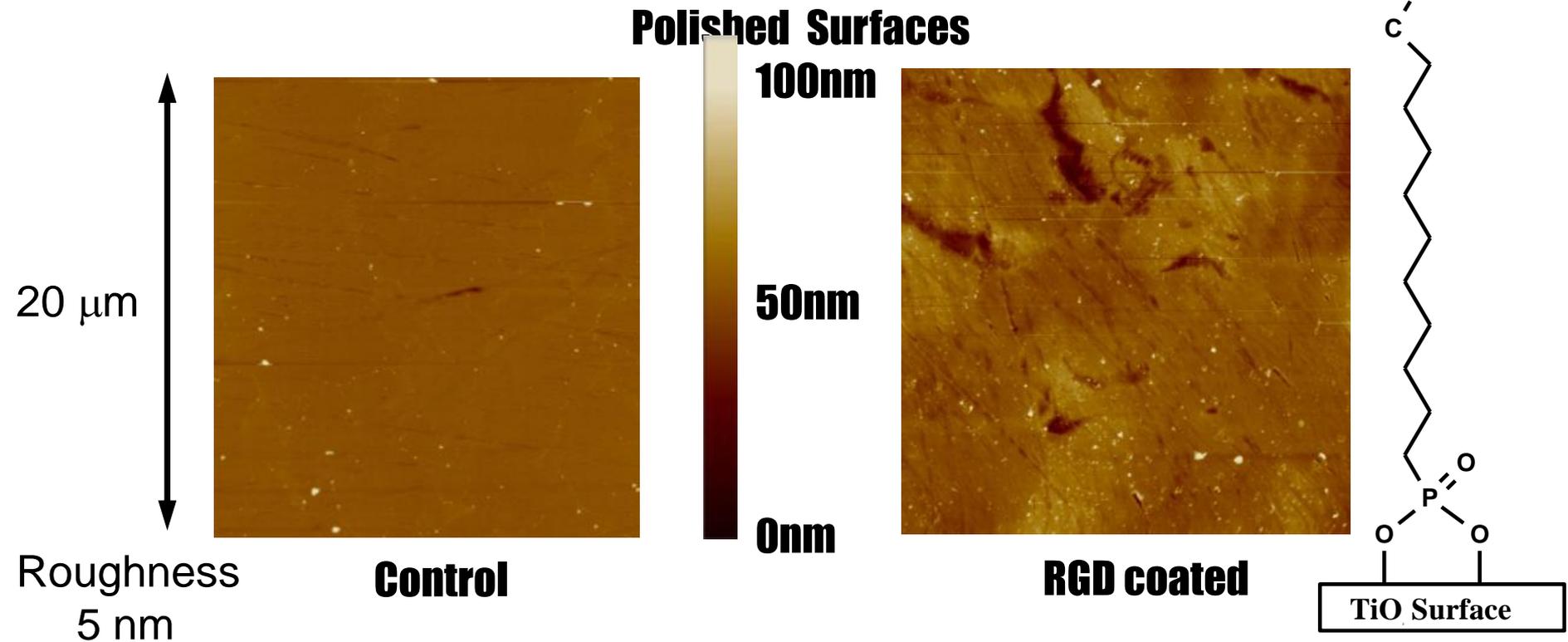
Cellular Adhesion Apparatus



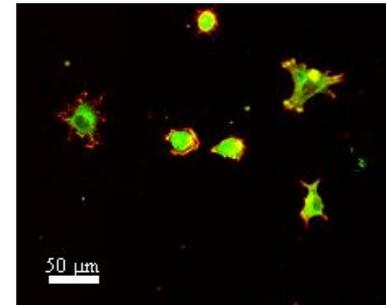
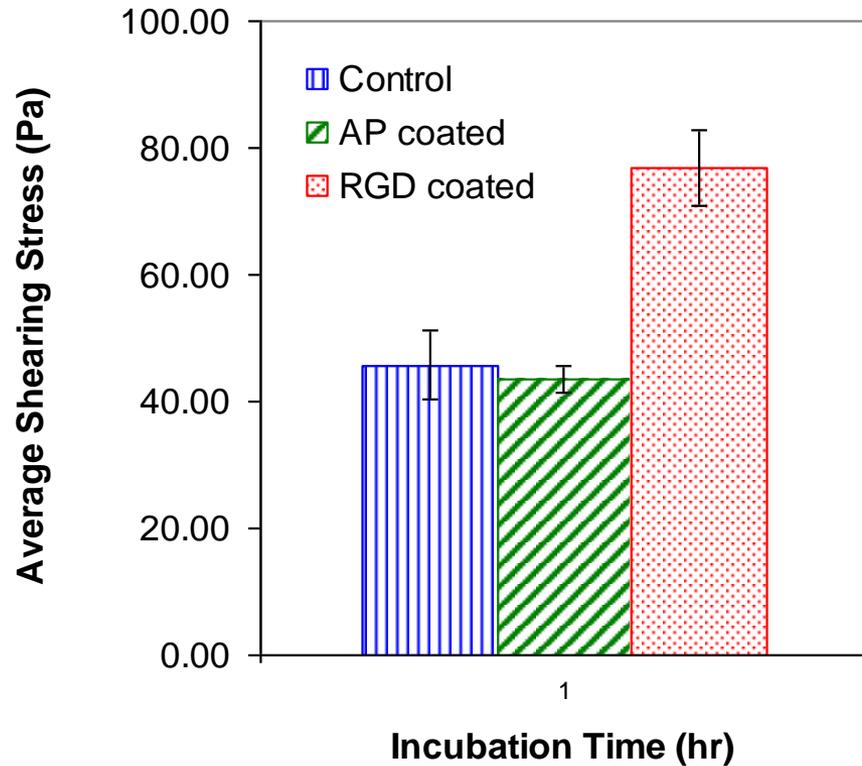
- Interaction between cell-cell and cell extracellular matrix are by specific contacts of adhesion molecules
- Cells in culture often form focal adhesion sites, a specialized and discrete region of the plasma membrane
- Cell viscoelastic deformability is determined largely by the composite shell envelope and cell cytoskeleton

Surface Preparation

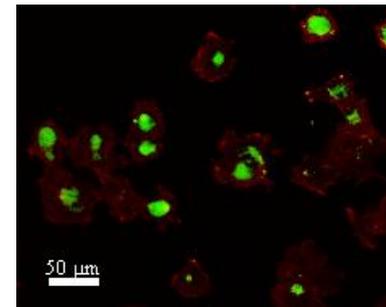
- Polishing
- AFM
- RGD-Coating



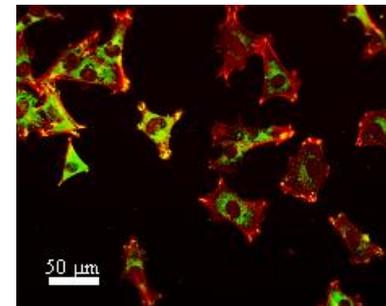
Interfacial Shear Strength Measurement



Control



AP coated

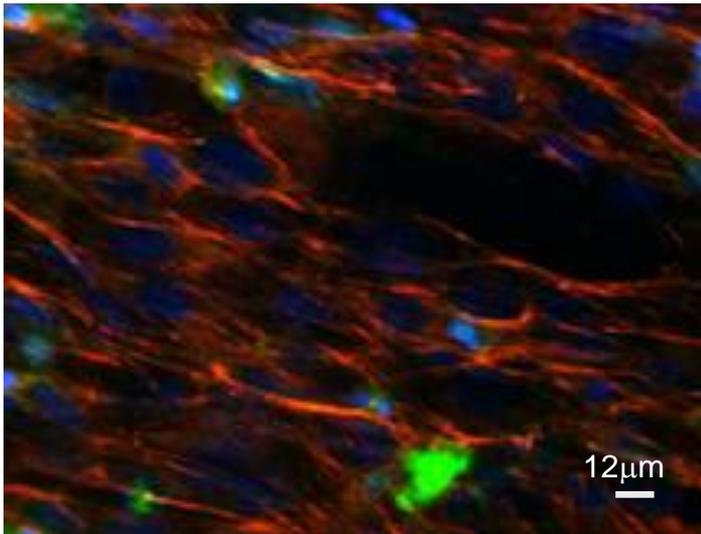


RGD coated

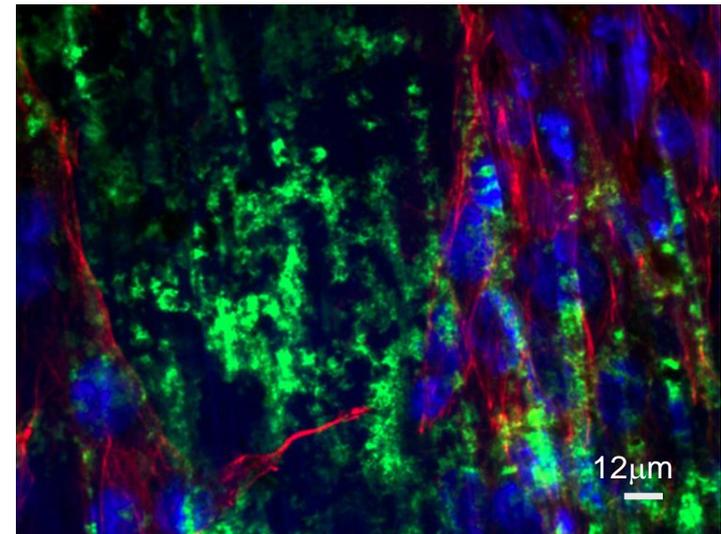
Effects of RGD Coating

- Short term effects of RGD coating:
 - Increased spreading and cellular adhesion
 - Increased protein organization of the cytoskeleton
- Previous studies indicate long term effects (mineralization):
- Clinical studies very promising

Control - 7 day



RGD - 7 day

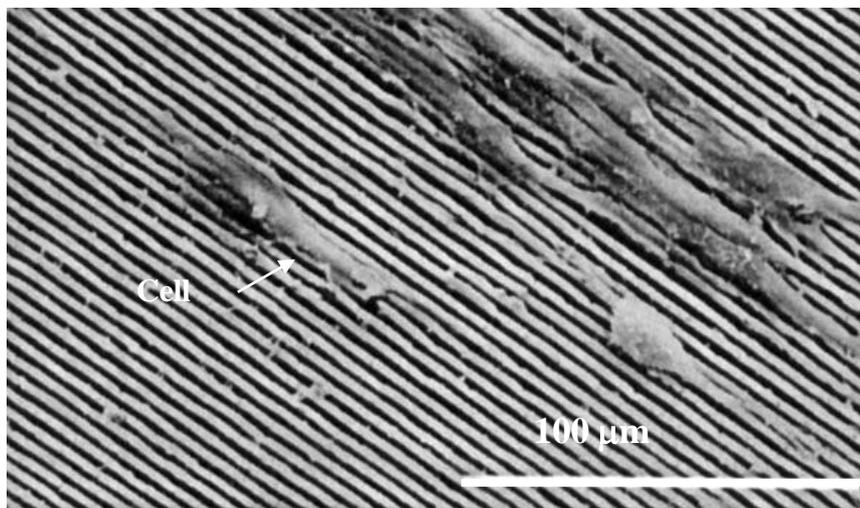


Stained for actin (red), nucleus (blue), hydroxyapatite (green)

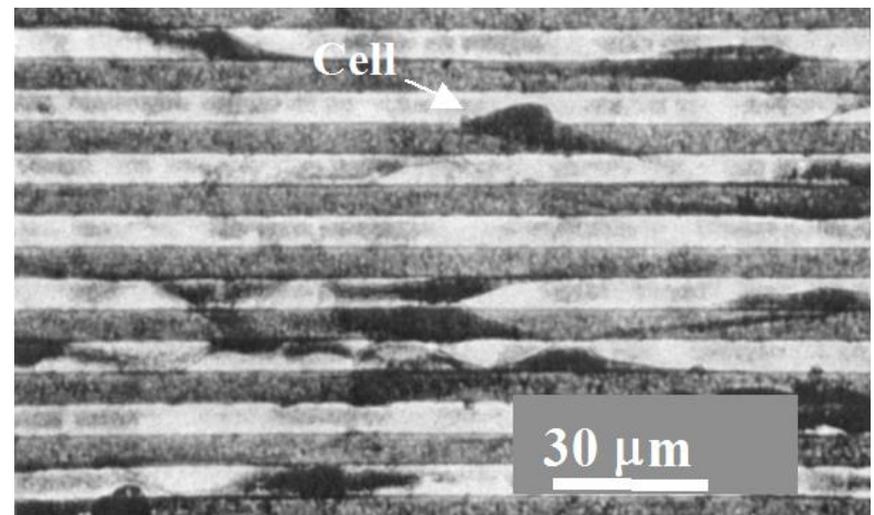
Micro-Groove Geometry and Cell/Surface Interactions

- Cells can undergo contact guidance when in contact with micro-grooved geometries
- This depends on the size of the grooves relative to the size of the cells
- Contact guidance has implications for wound healing and scar tissue formation

2 μm Micro-Grooves

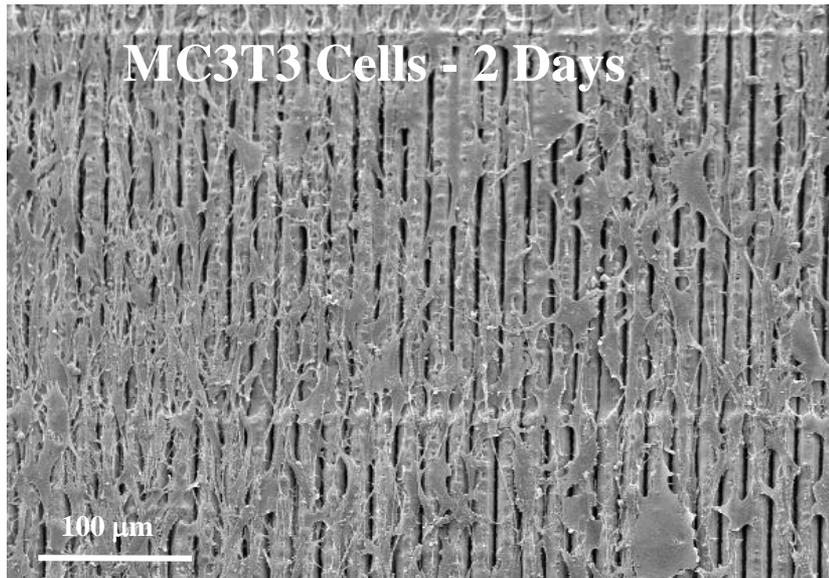


12 μm Micro-Grooves

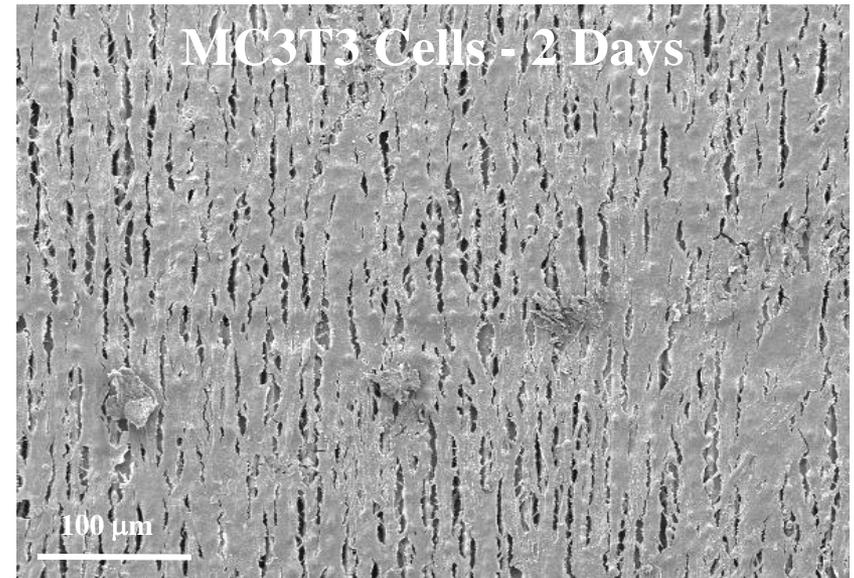


Laser Textured Surfaces - Cell/Surface Interactions

8 μm Grooves

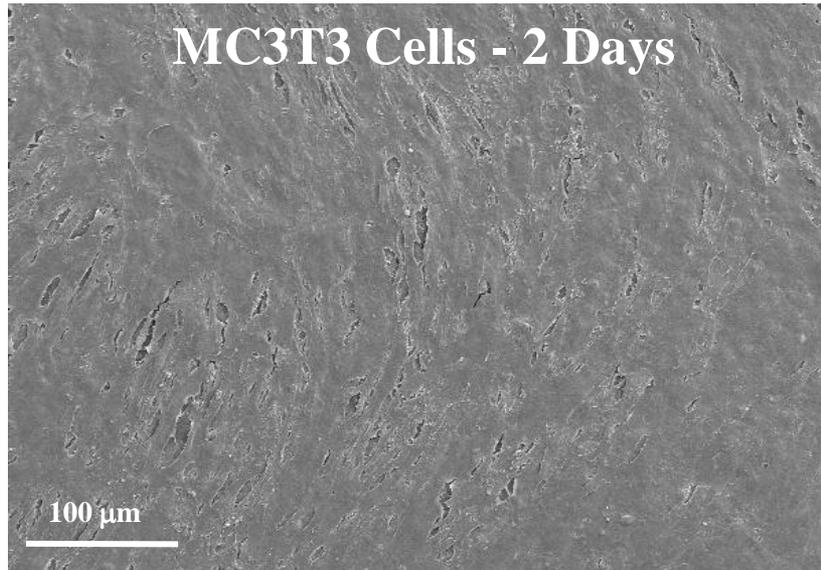


12 μm Grooves

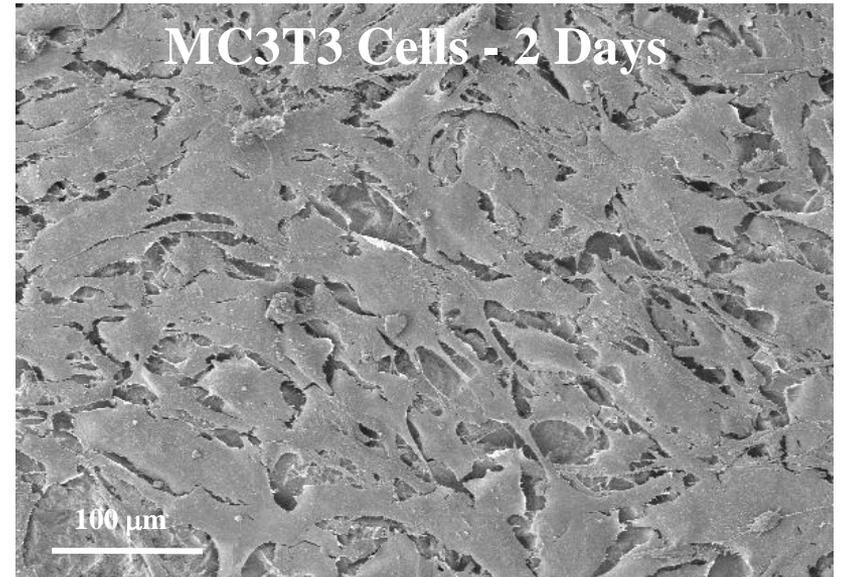


Surface Texture - Cell/Surface Interactions

Polished



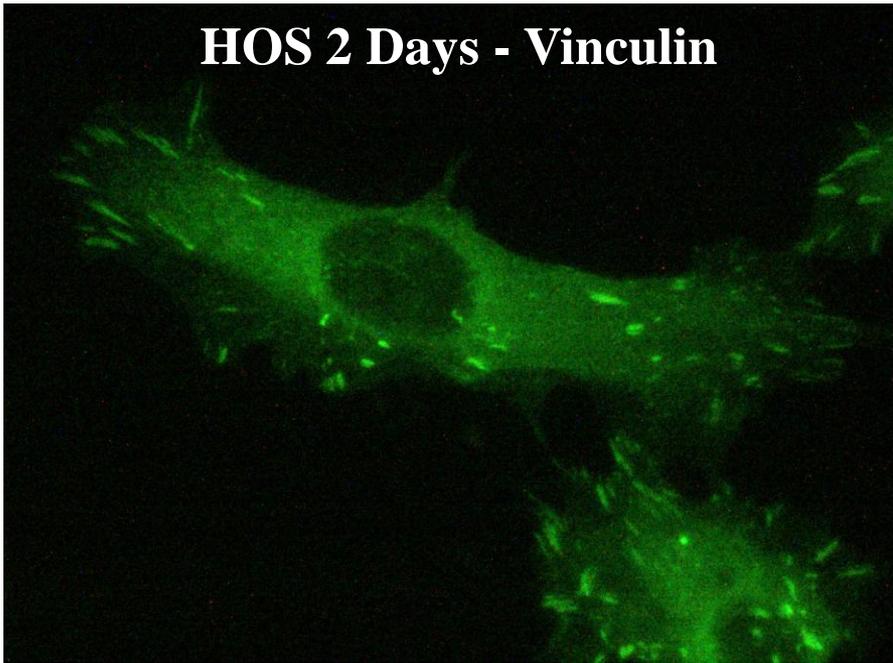
Al₂O₃ Blasted



Surface Texture – UV Laser Textured Surfaces IF Staining

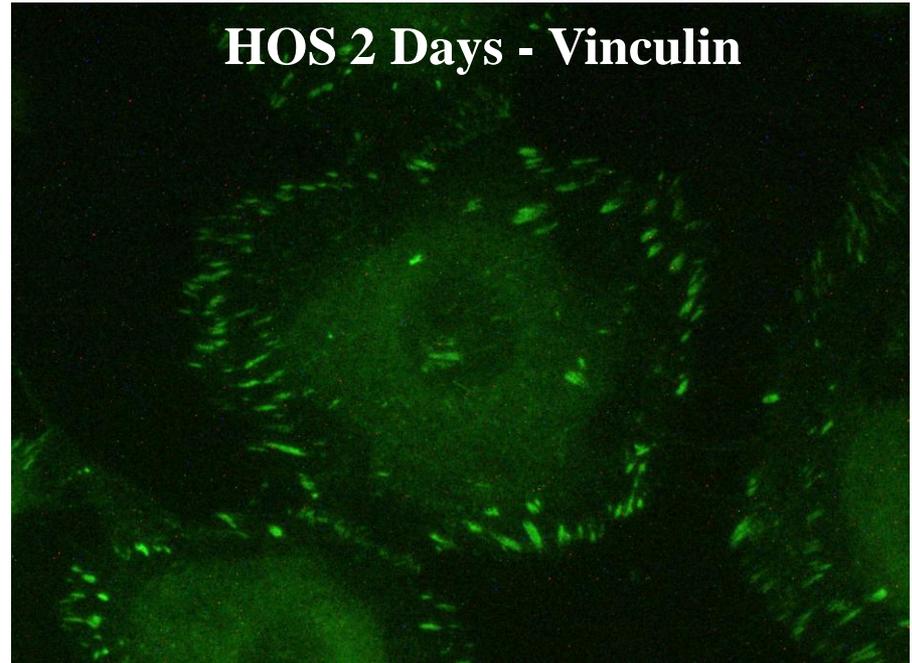
11 μm Laser-Grooved Surface

HOS 2 Days - Vinculin



Polished Surface

HOS 2 Days - Vinculin

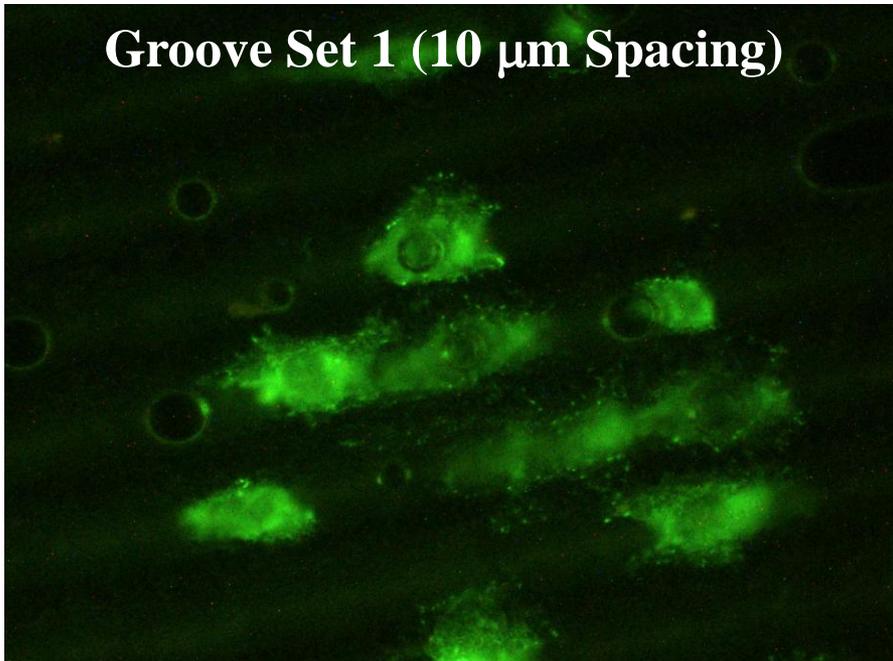


Surface Texture – UV Laser Textured Surfaces

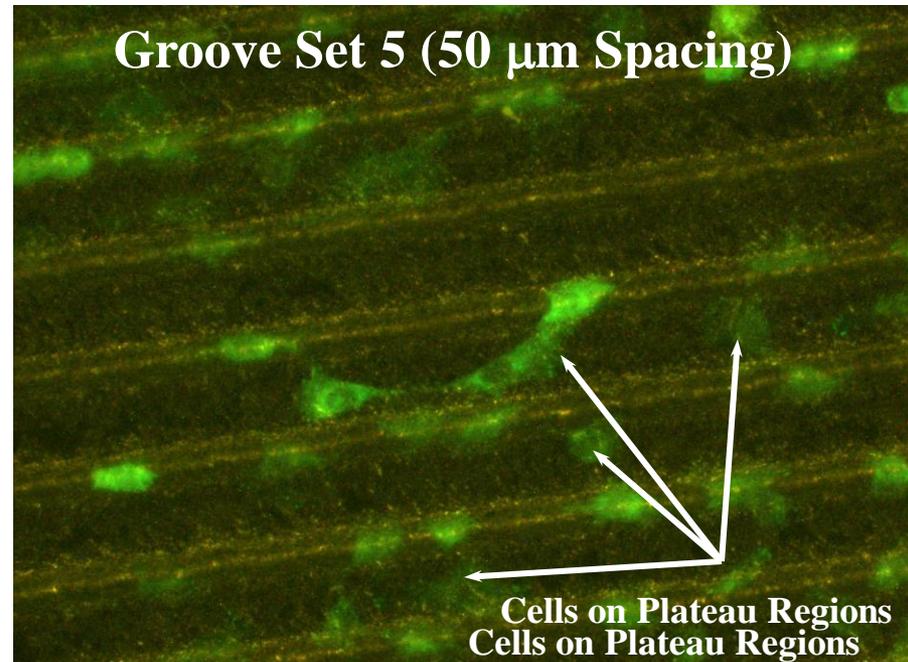
Cell/Surface Interactions

- HOS cells cultured on groove set 1 (10 μm spacing) lie within micro-grooves – high level of contact guidance.
- HOS cells cultured on groove set 5 (50 μm spacing) display a moderate level of contact guidance – some cells span across plateau regions.

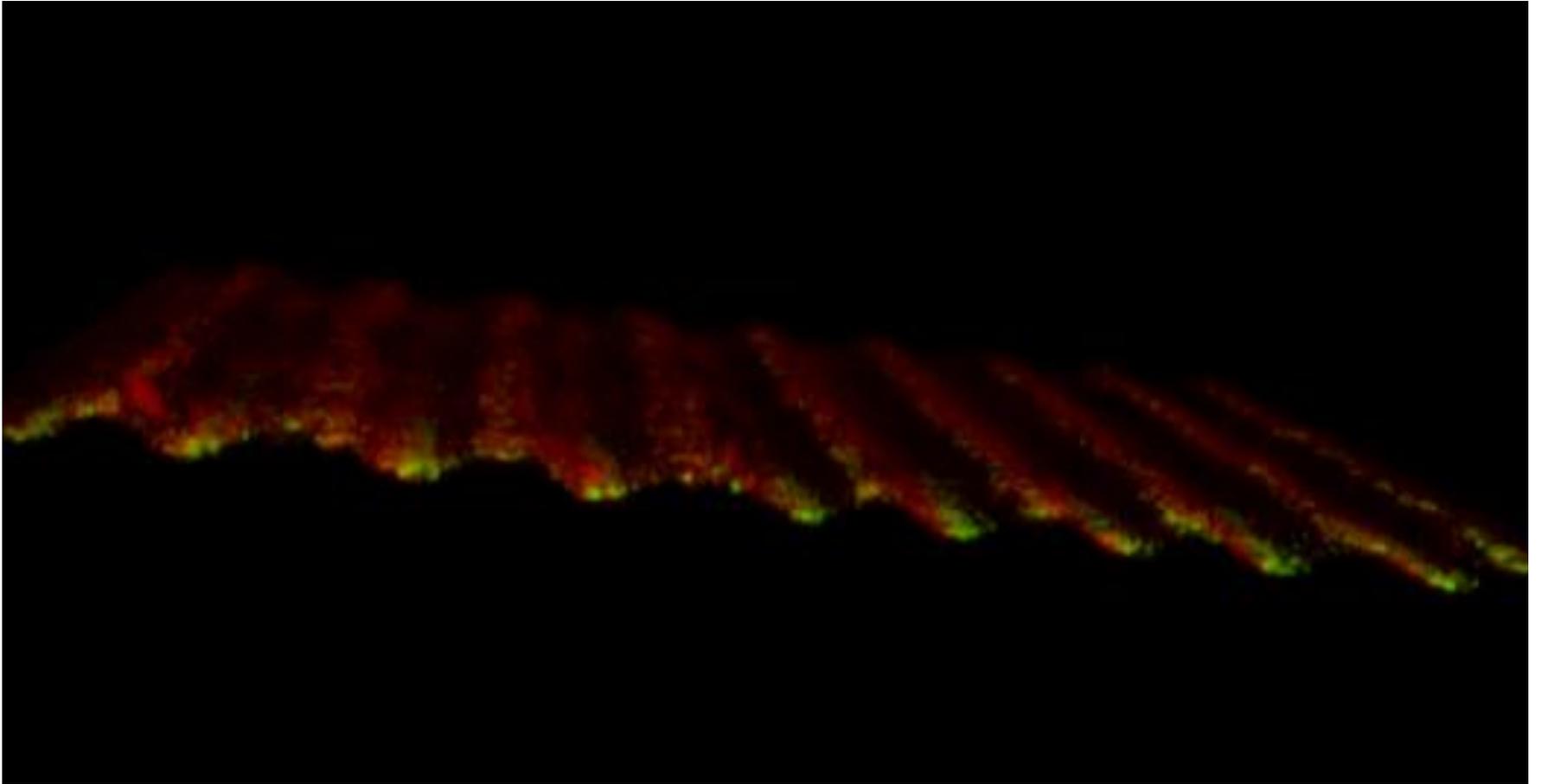
Groove Set 1 (10 μm Spacing)

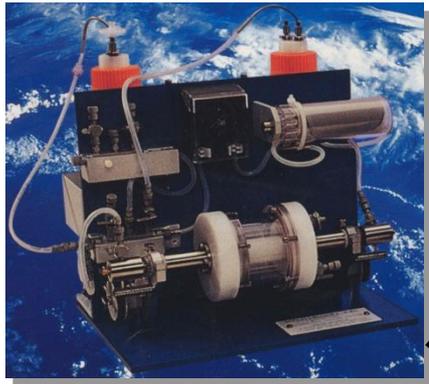


Groove Set 5 (50 μm Spacing)

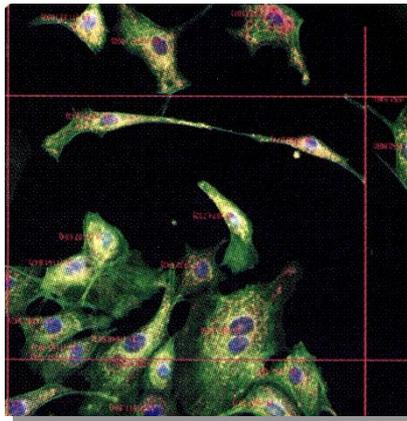


3-D View (Horizontal, 10micron)





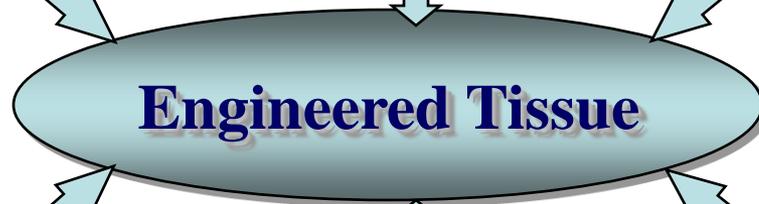
Bioreactor Design



Cells



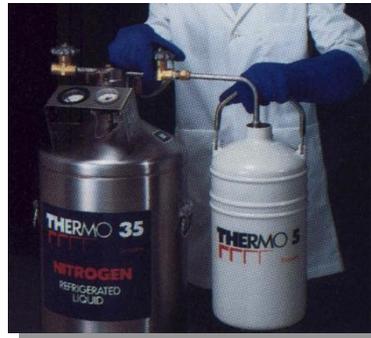
Scaffolds



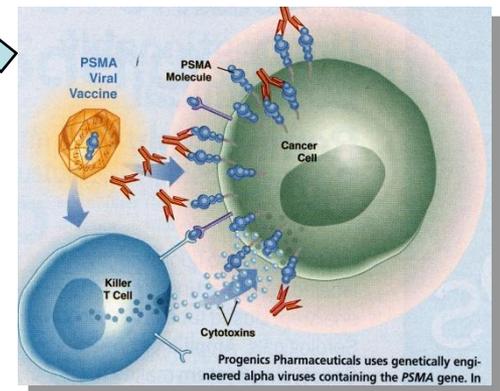
Engineered Tissue



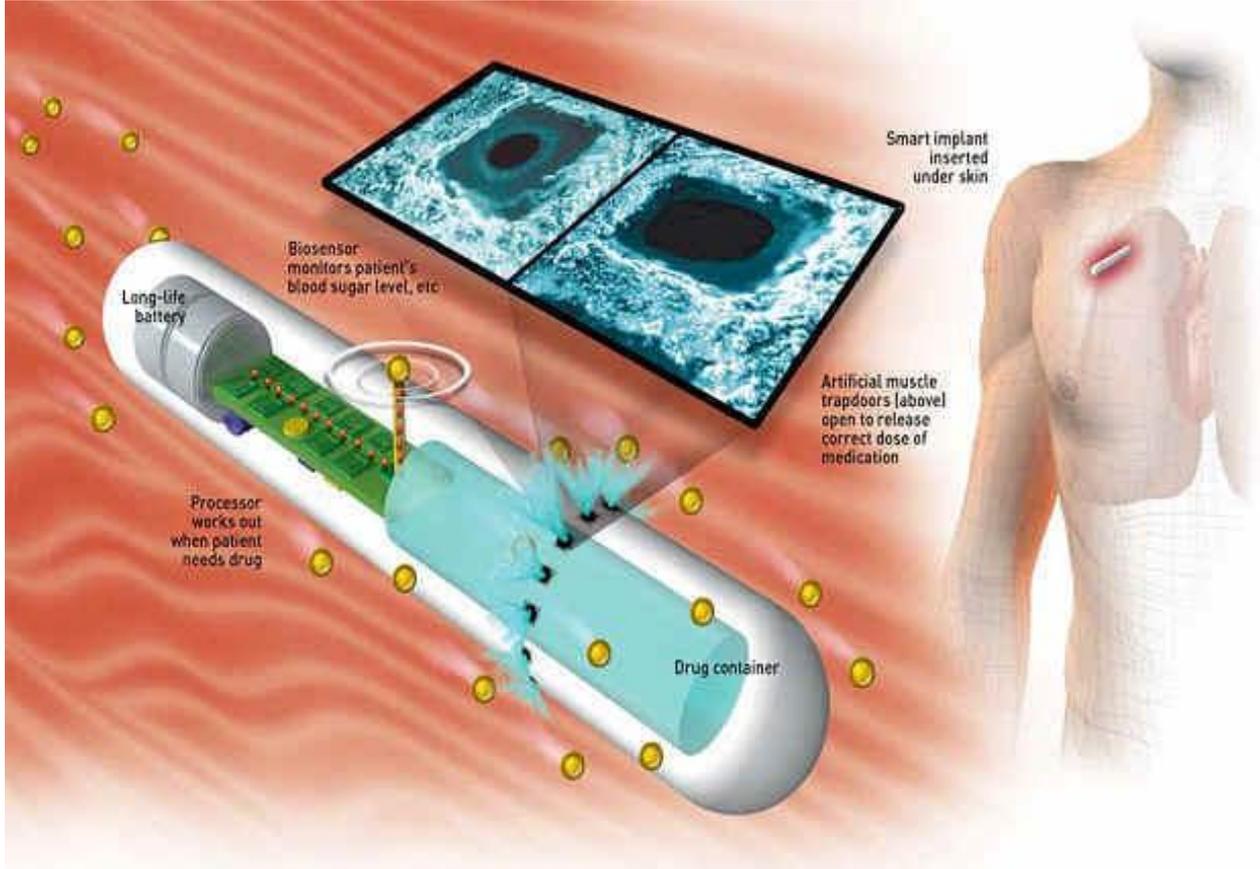
Upscaling



Preservation

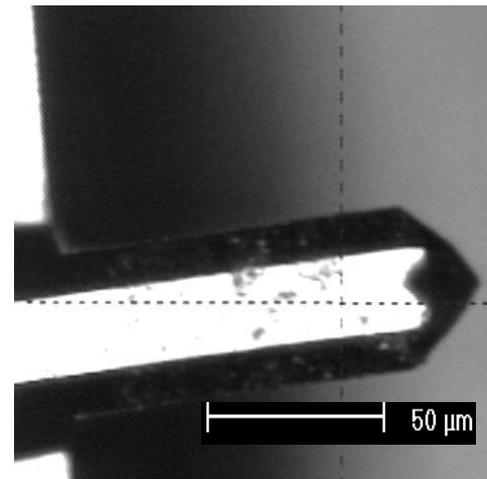


Immunoisolation/
Compatibility



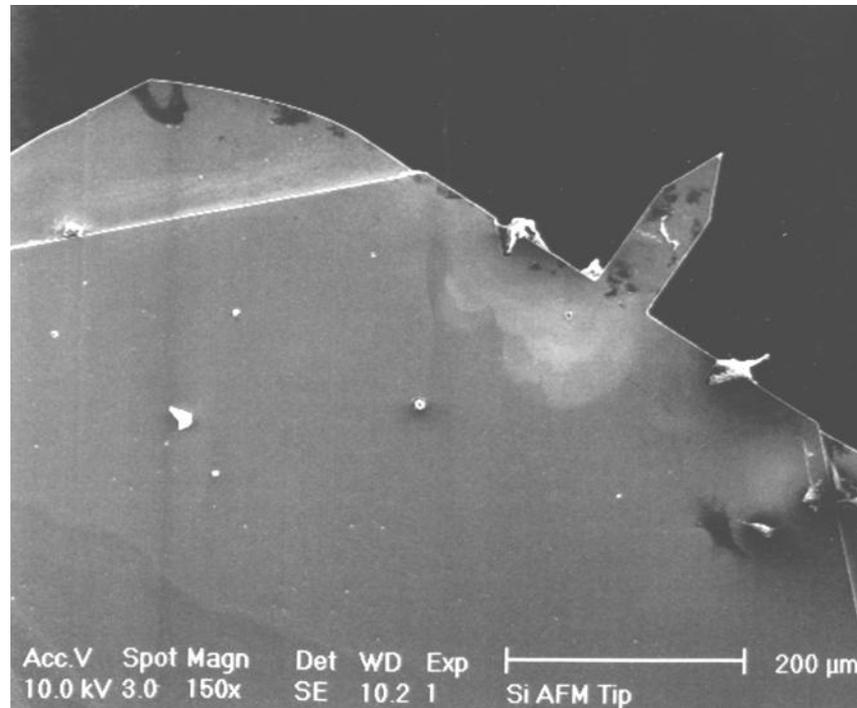
A FEW METHODS FOR DETECTING CANCER

- View under a microscope at high magnification
- Use a biochemical assay to reveal cells
- Use a bioMEMS cell detector e.g. a cantilevered MEMS structure
- External imaging system, e.g. MRI

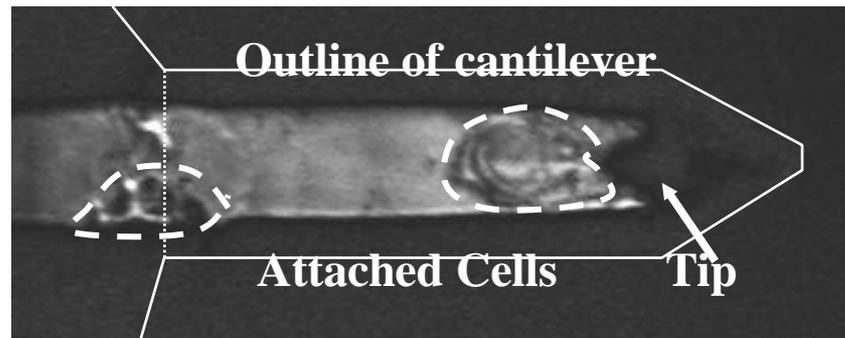


Single HOS Cell on Si Cantilever in AFM

Single cell on Si Cantilever



CELL DETECTION ON CANTILEVER



Cantilever No. 17

Initial Frequency: 263.36 KHz

Spring constant: 44.86 N/m

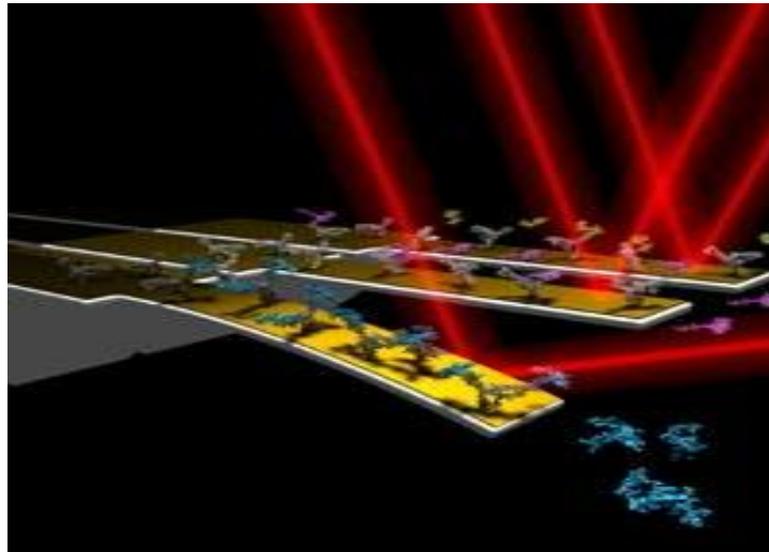
Final Frequency: 261.59 KHz

Difference: 1.77 KHz

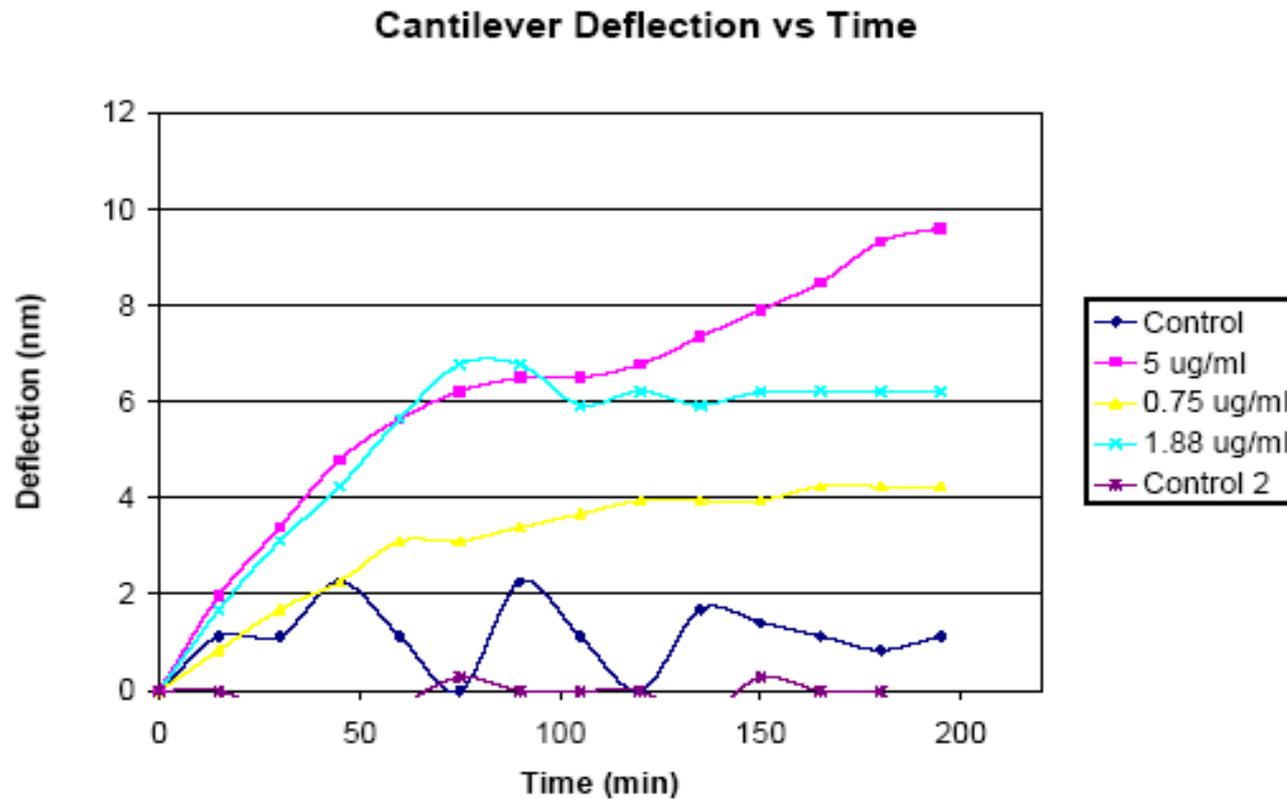
- Cantilever shows the presence of two cells
 - one attached near the tip, the other is at the base of the cantilever

Antibody/Antigen Interactions

- Antibody/antigen interactions cause surface stresses to develop
- These surface stresses are the result of new conformations of molecular structures at the surface
- Interactions between Vimentin antibodies and antigens gives rise to surface stress and cantilever deflection



Cantilever Deflection data



THE FUTURE OF CANTILEVERED BIOMEMS STRUCTURES – BIOMOLECULAR DETECTION

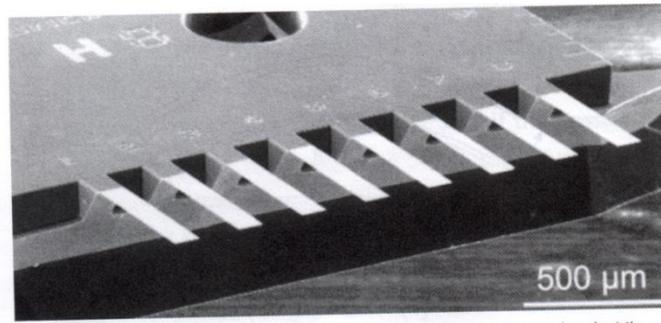
- Research will lead to future cantilevered bioMEMS structures
- Devices may be resonating devices for improved sensitivity
- However, non-resonating devices can also be used
- Multifunctional structures emerging with multiple cantilevers

Functionalized Cantilever

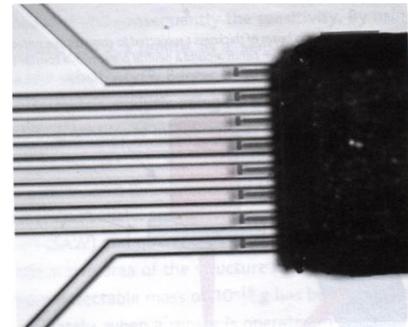


- DNA
- Folic Acid
- Antibodies

Microcantilever Array



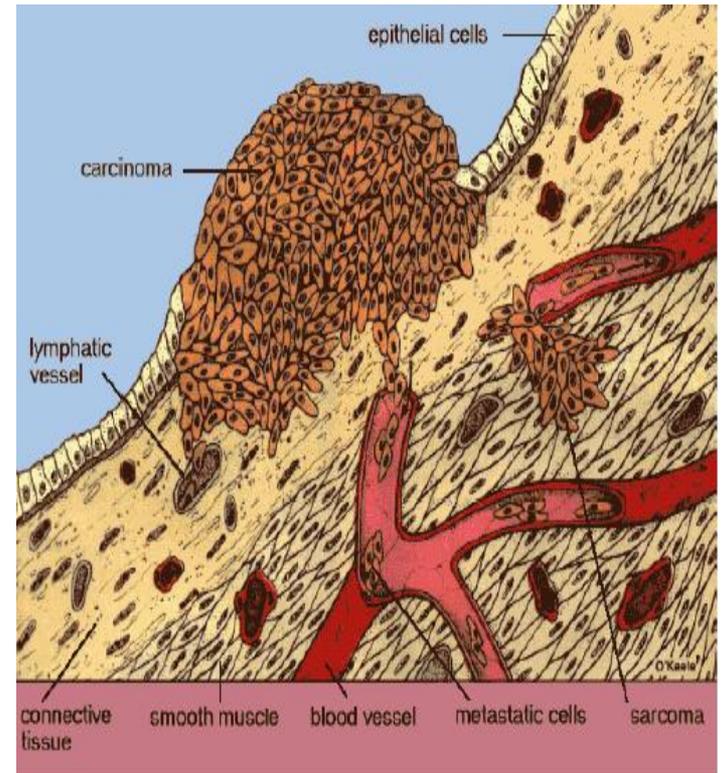
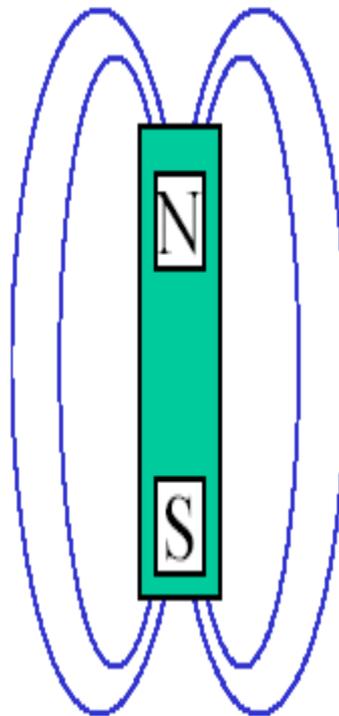
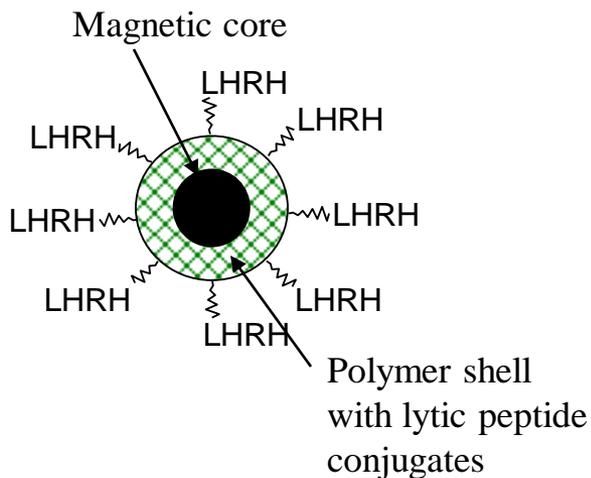
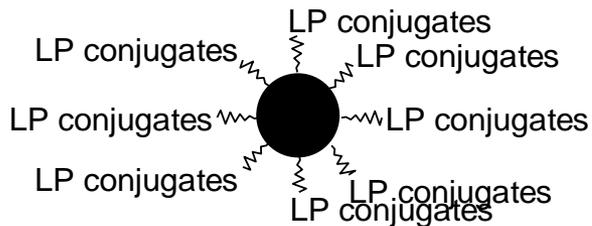
Packaging





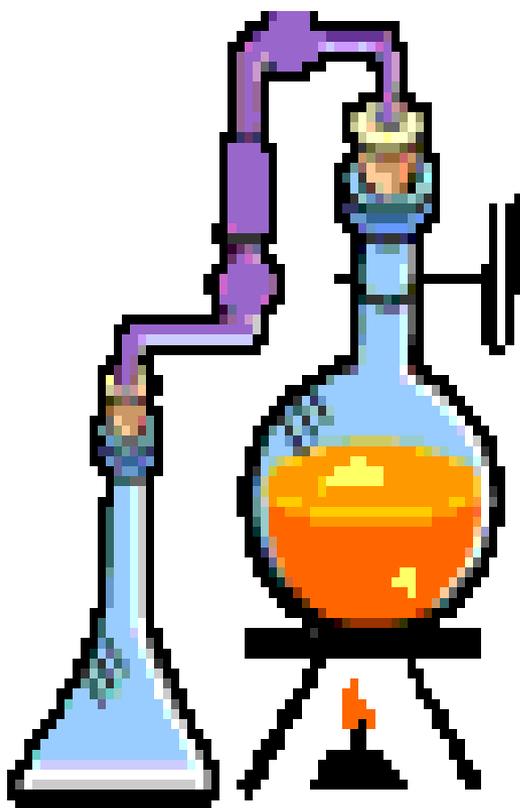
Our Approach to Early Cancer Detection and Treatment!

A novel use of magnetic fields and magnetic particles to deliver therapeutic drugs at the desired time in the correct dosage to the correct site in the human body.





Wet Chemical Synthesis of Nano-particles

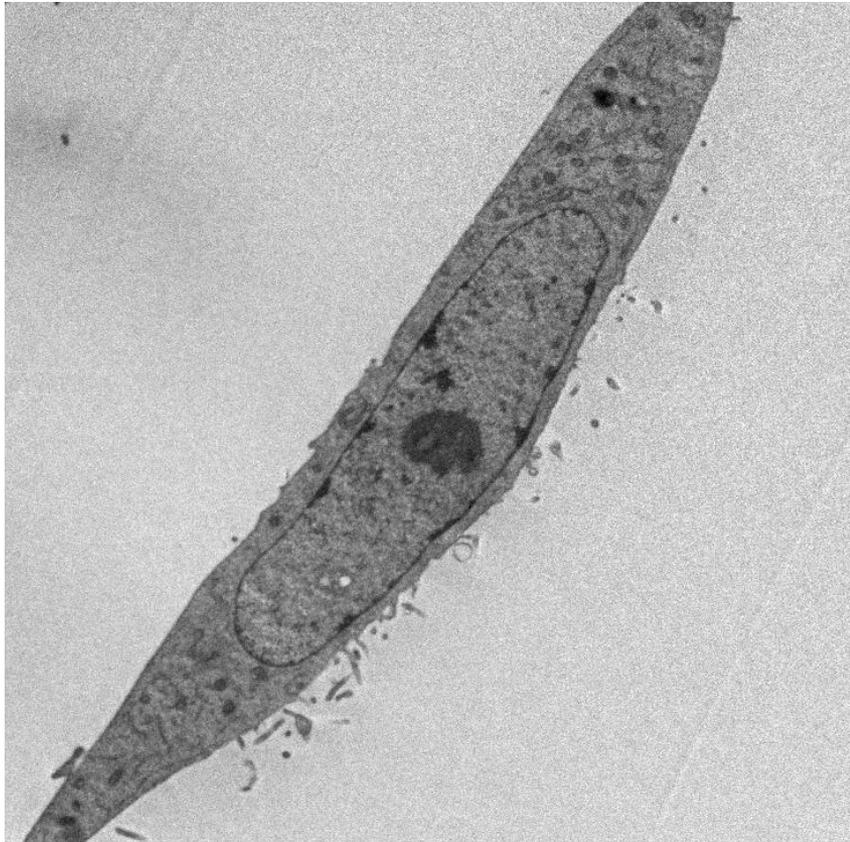


- Metallic, polymeric and metal-polymer Nano-particles using bottom-up approaches
- Novel Micro reactor technology for scale-up and controlled synthesis
- Synchrotron radiation based X-ray absorption Spectroscopic characterization
- Capability to attach bio-molecules

In-Vitro Experiments

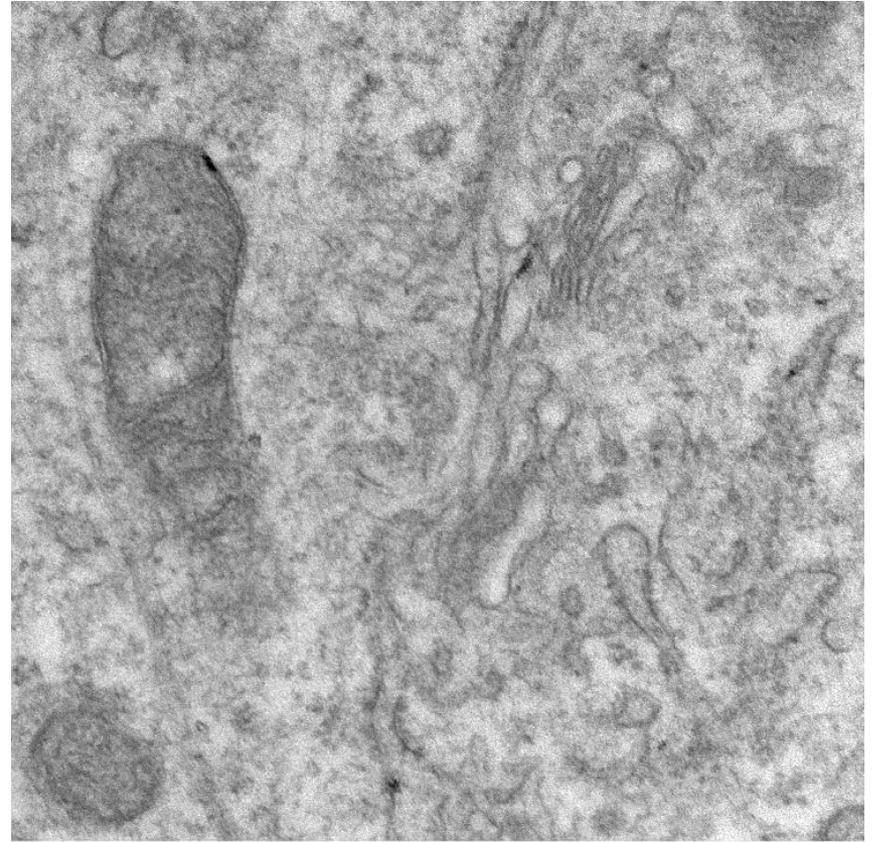
- Studied attachment of nano-particles in cell culture experiments
- Studied effects of temperature and time
- Imaging done using TEM after fixing
- Studies conducted on breast cancer cells with LHRH receptors
 - Unconjugated nanoparticles
 - LHRH-coated nanoparticles

TEM Images of Breast Cancer Cells (Control)



Control-52.tif
In Vitro

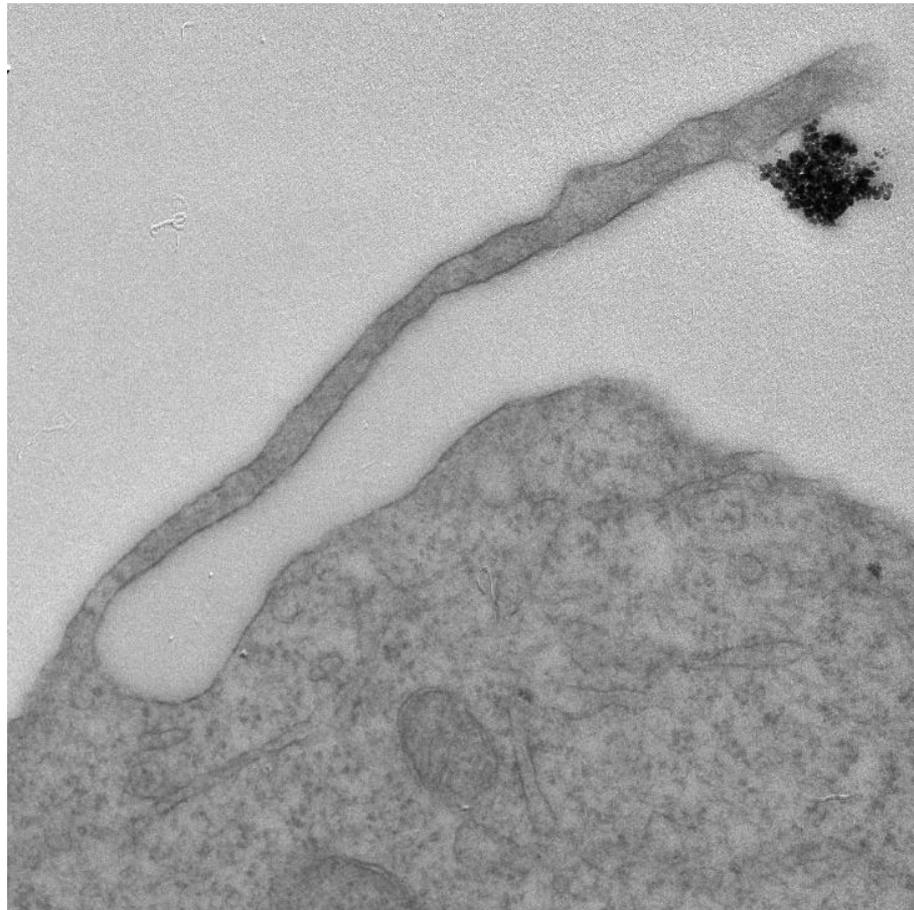
2 microns



Control-05.tif
In Vitro

100 nm

SPION Uptake - 37 C for 30 Minutes

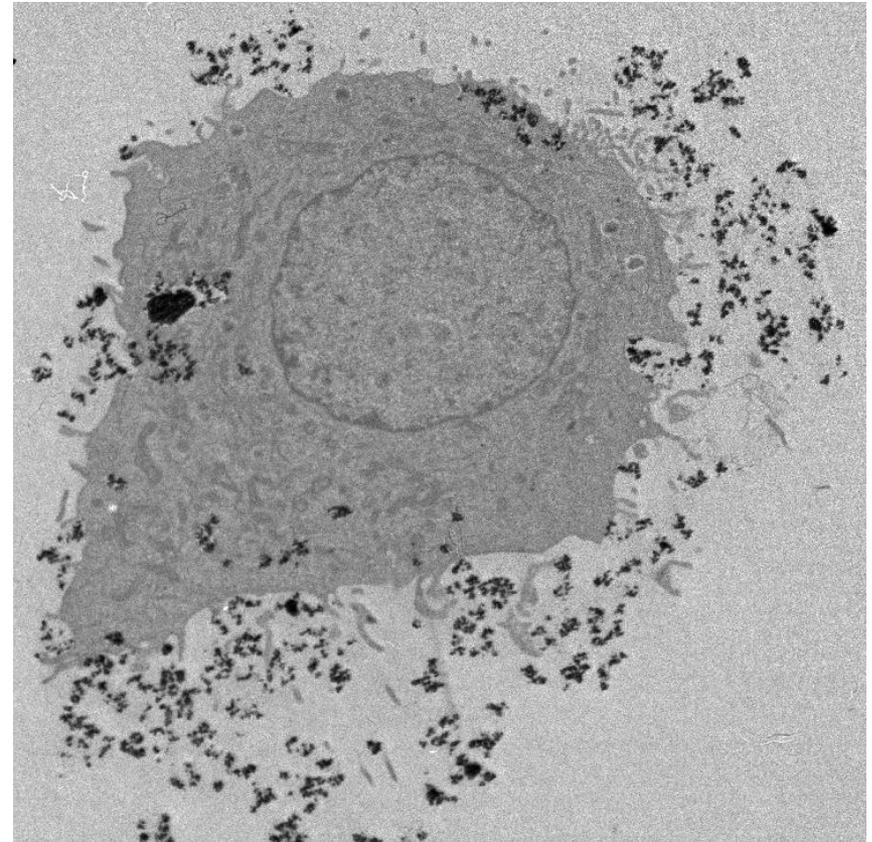


InV1032-48.tif
In Vitro

100 nm

LHRH-SPION Uptake - 37 C for 3 Hours

- MNPs-LHRH, 37 C, 3 Hr
- Note encryption process by which cells attach
- Engulfed cells carried within the cell
- Excreted or egested within 30 days

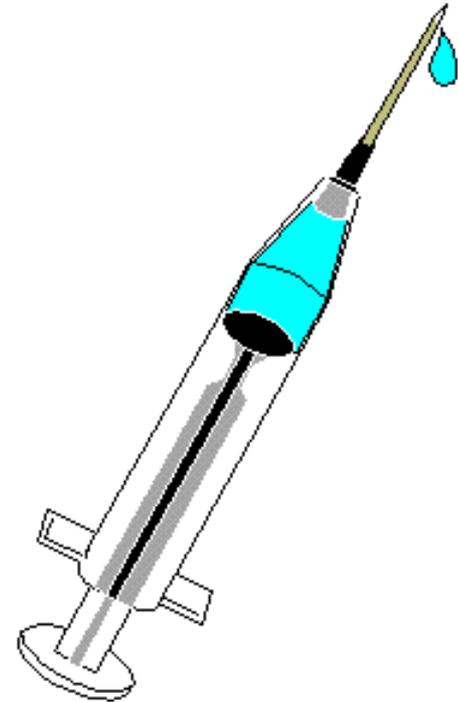


InV10312-30.tif
In Vitro

2 microns

In-Vivo Experiments

- Mice injected in 4 different ways:
 1. LHRH nanoparticles
 2. saline solution
 3. nanoparticles
 4. LHRH nanoparticles but with mice that do not contain breast tumor



Materials Characterization of Organs (TEM and Histology)

Organs obtained:

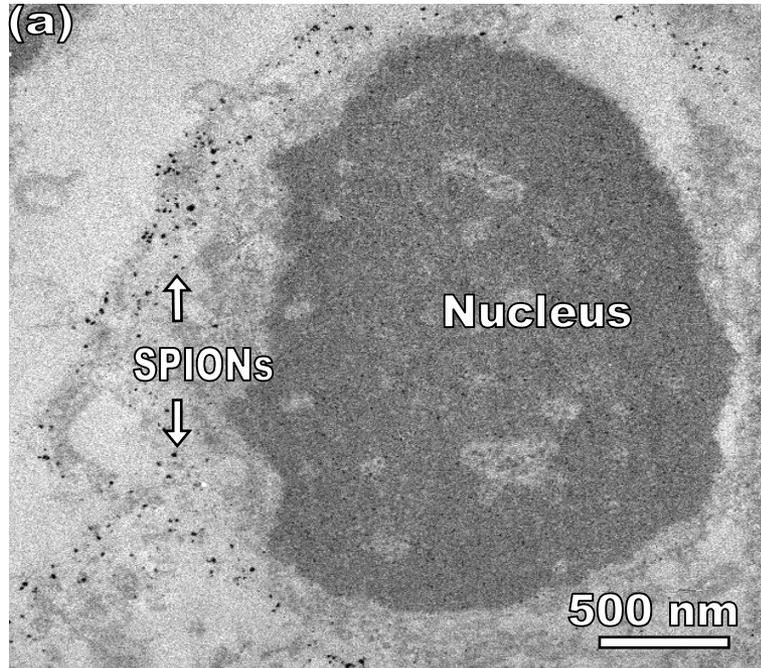
- breast or prostate tumor
- Kidney
- Lung
- Liver



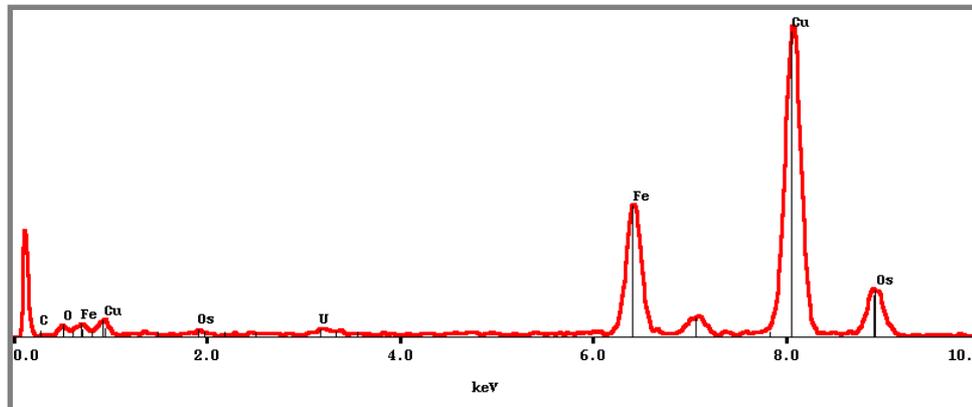
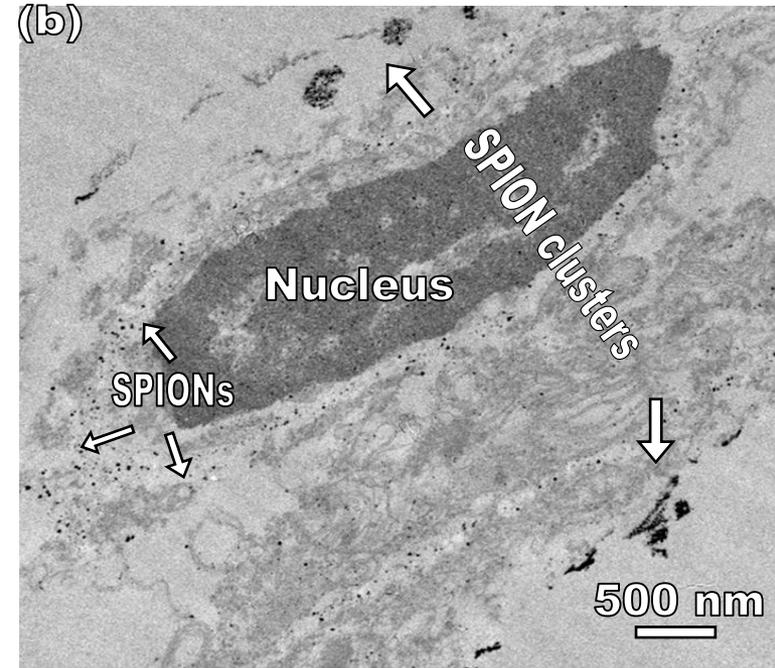
Ensure that the nanoparticles do not accumulate in other major organs.

SPION/SPION-LHRH in Breast Tumor

SPION in Tumor

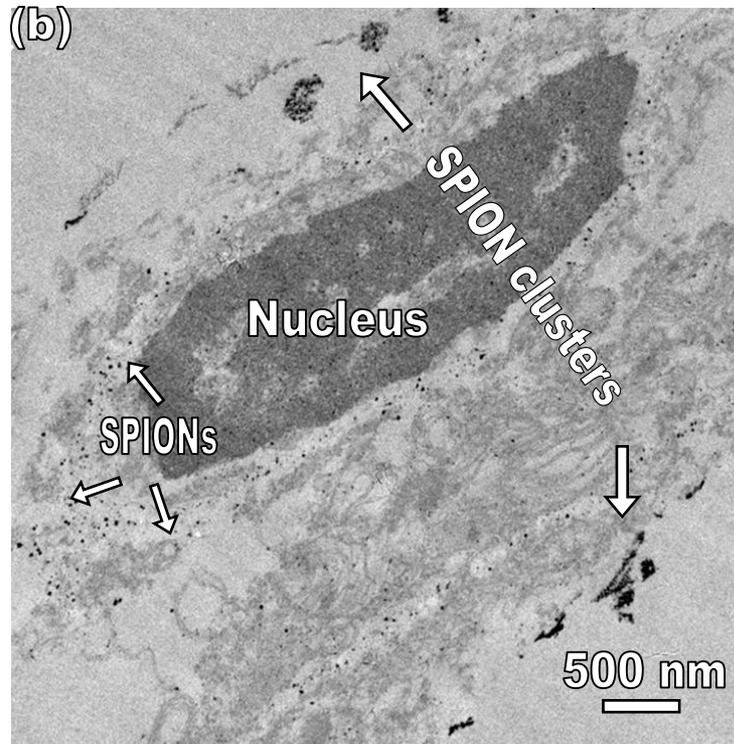


LHRH-SPION in Tumor

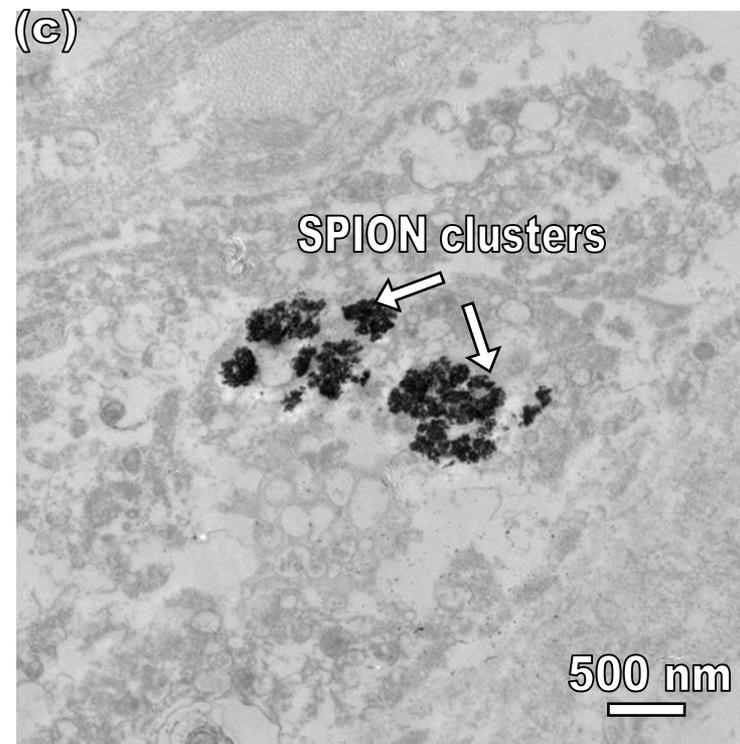


SPION/SPION-LHRH in Breast Tumor

LHRH-SPION in Tumor

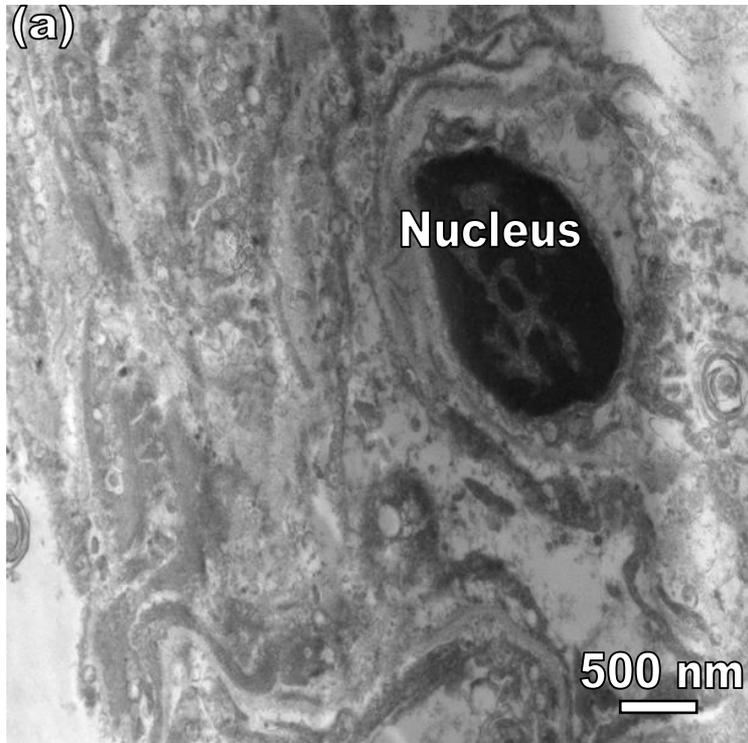


LHRH-SPION in Tumor

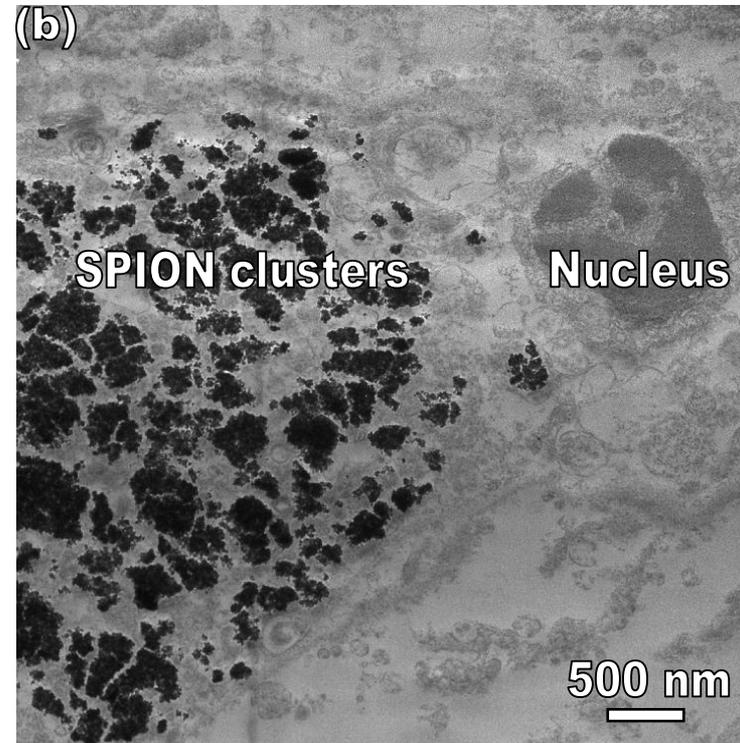


SPION in Lung

SPION in Lung

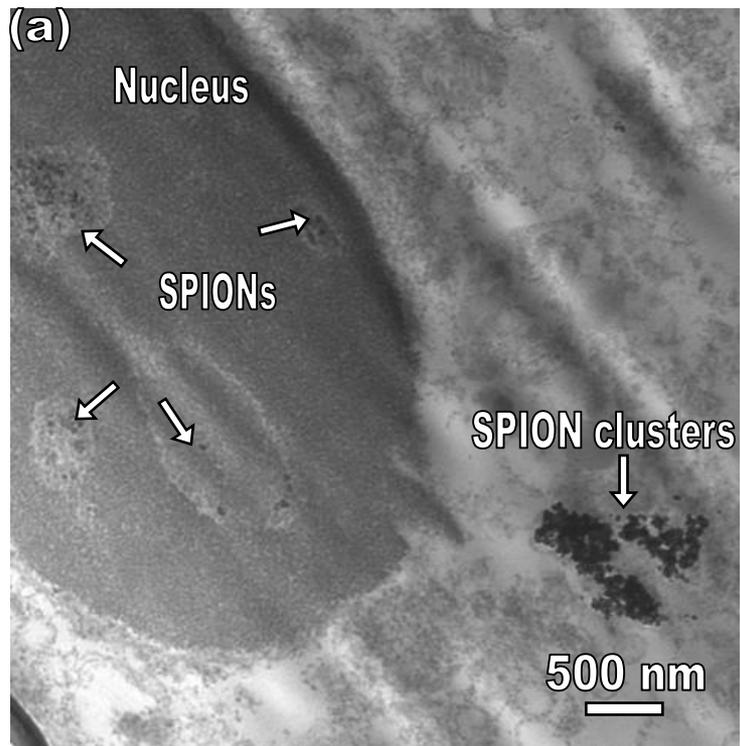


LHRH-SPION in Lung

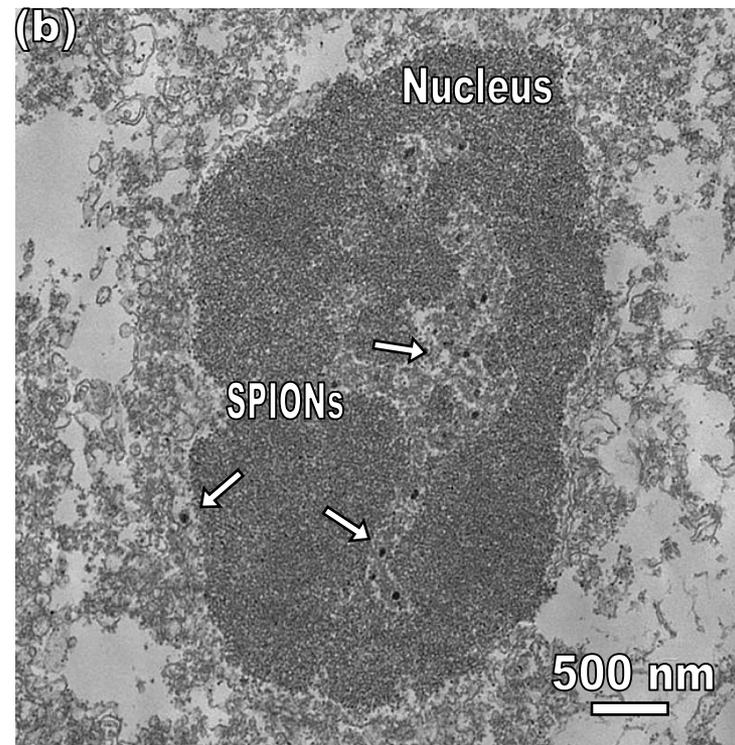


SPION/SPION-LHRH in Liver

SPION in Liver

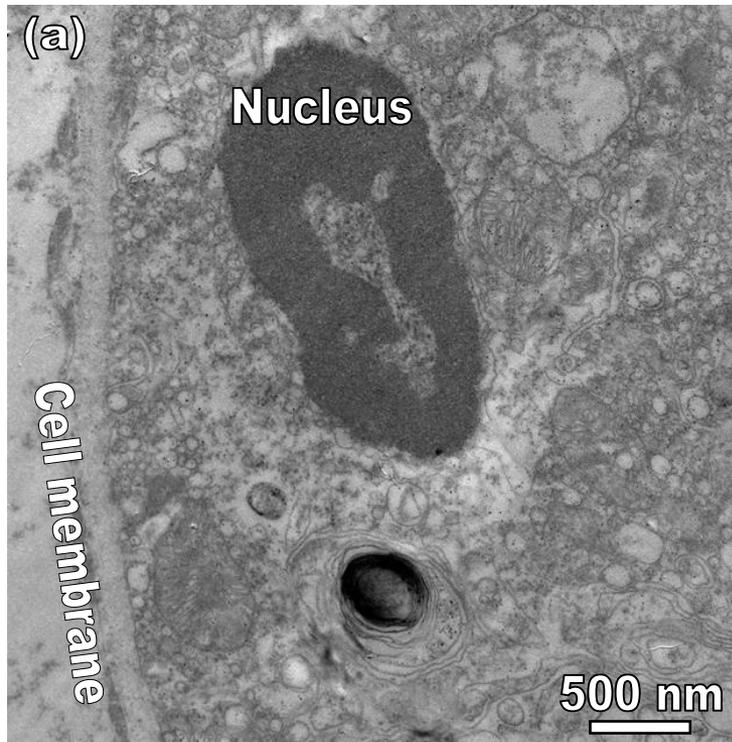


LHRH-SPION in Liver

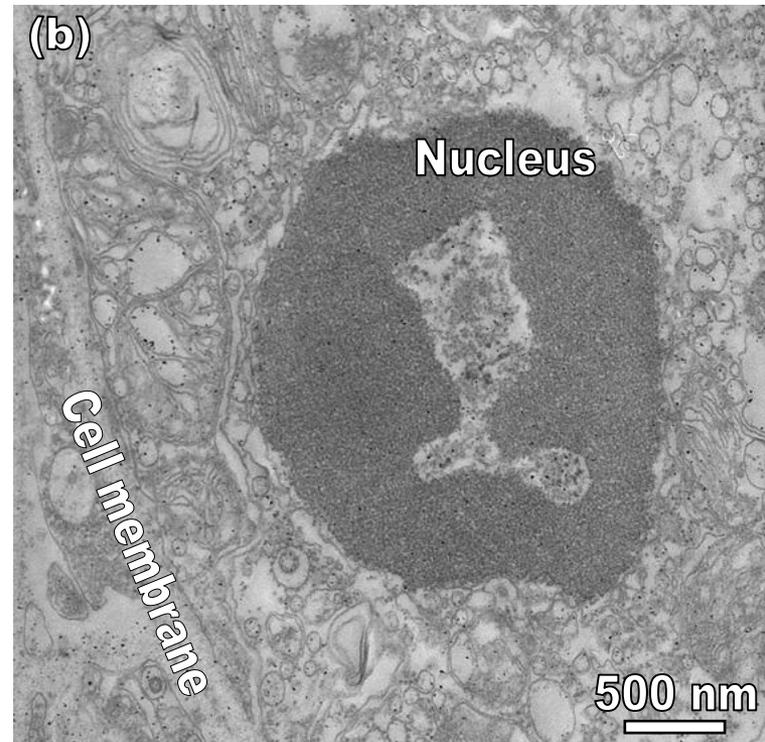


LHRH-SPION in Kidney

SPION in Kidney

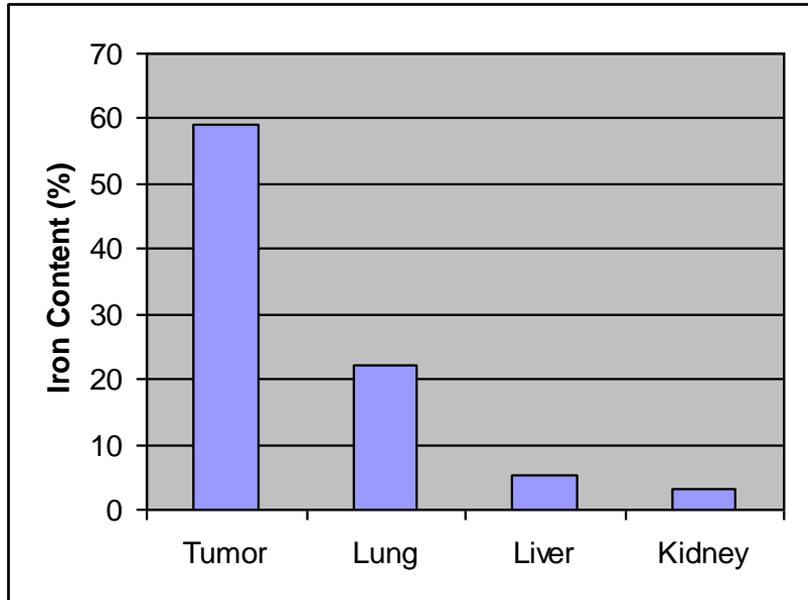


LHRH-SPION in Kidney

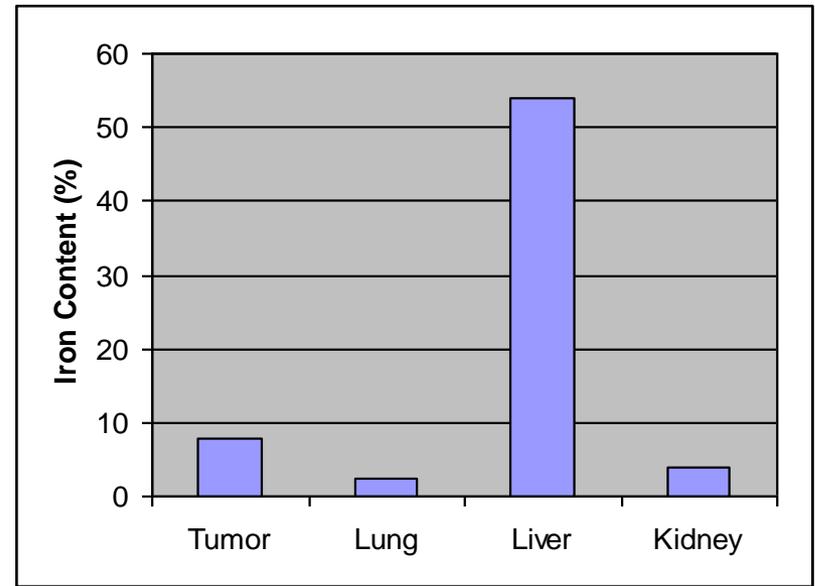


Biological Distribution of SPIONs

LHRH-SPION in Mouse

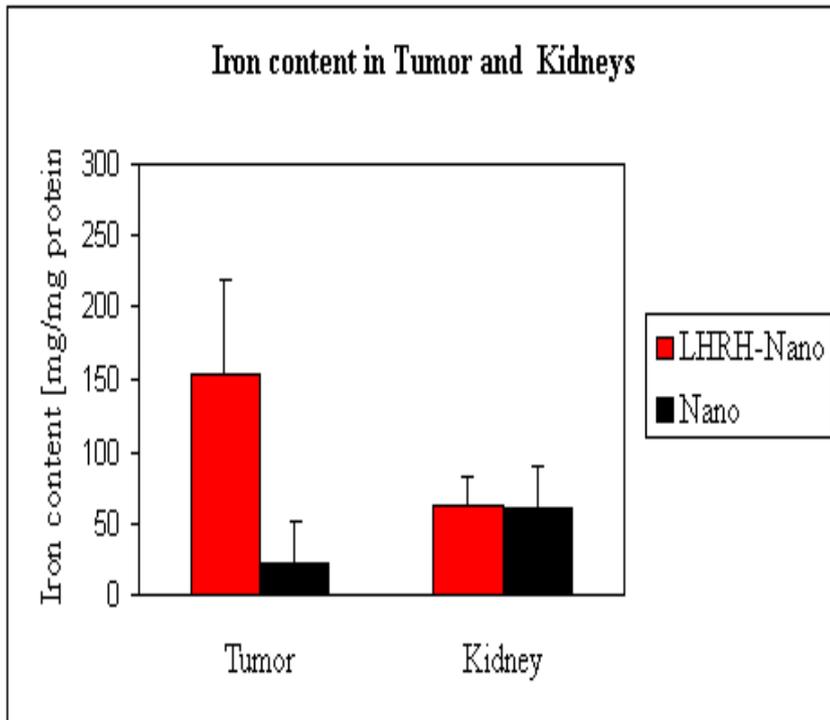


SPION in Mouse





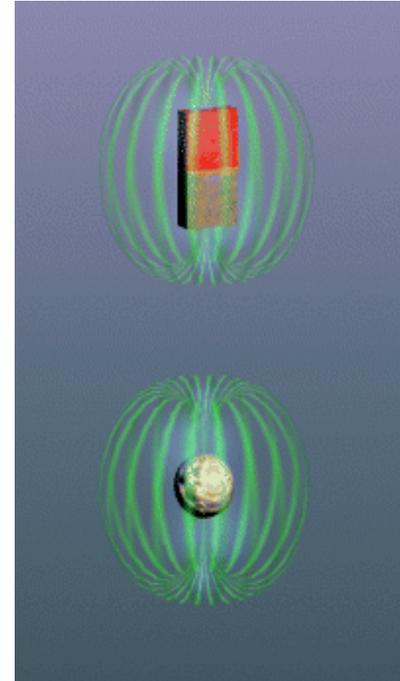
Targeted Destruction of Prostate Cancer in Balb/c athymic nude mice



- PC-3.luc Xenograft bearing male nude mice were used
- LHRH bound nanoparticles effectively bind to tumor
- Use of Nano-LHRH results in accumulation 68% of nanoparticles in tumor
- Distribution of iron in other tissues is being mapped

Fundamentals of Magnetic Resonance Imaging (MRI)

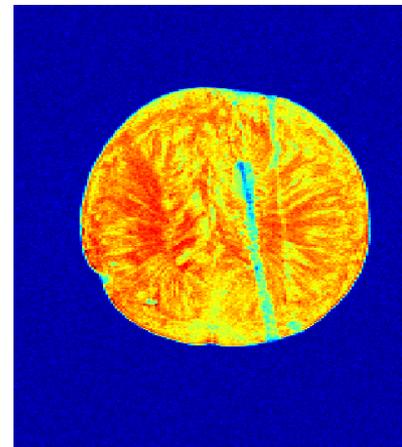
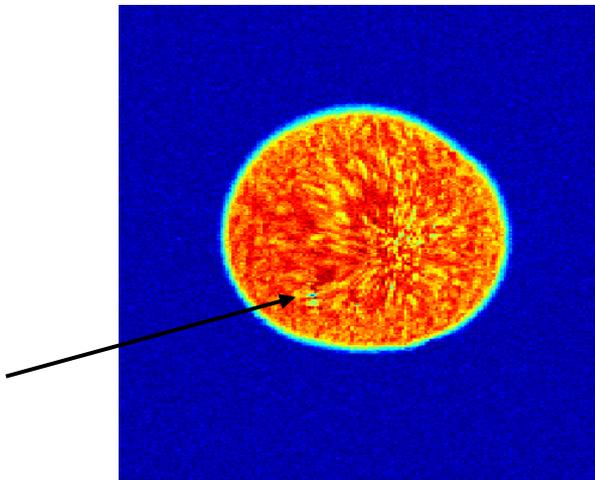
- Hydrogen atoms in water have a property called spin
- MRI generates a magnetic pulse that aligns all of the spins in a certain direction
- The magnetic resonances of the nuclei will cause differences in how they return to their normal spin state
- The MRI machine records the energy released as they realign at different times and generates an image
- A set of images are generated at certain small time intervals after the pulse sequence



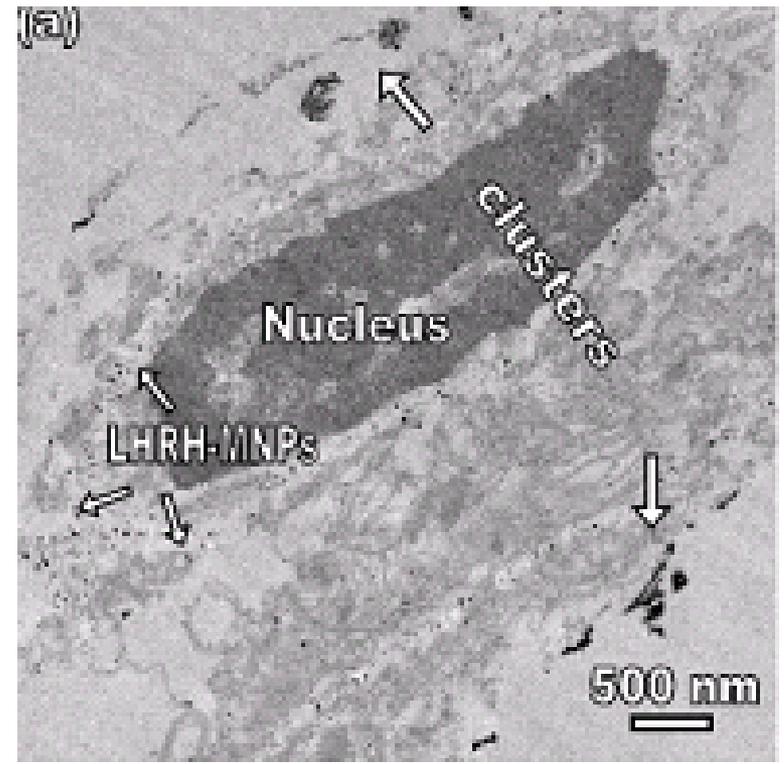
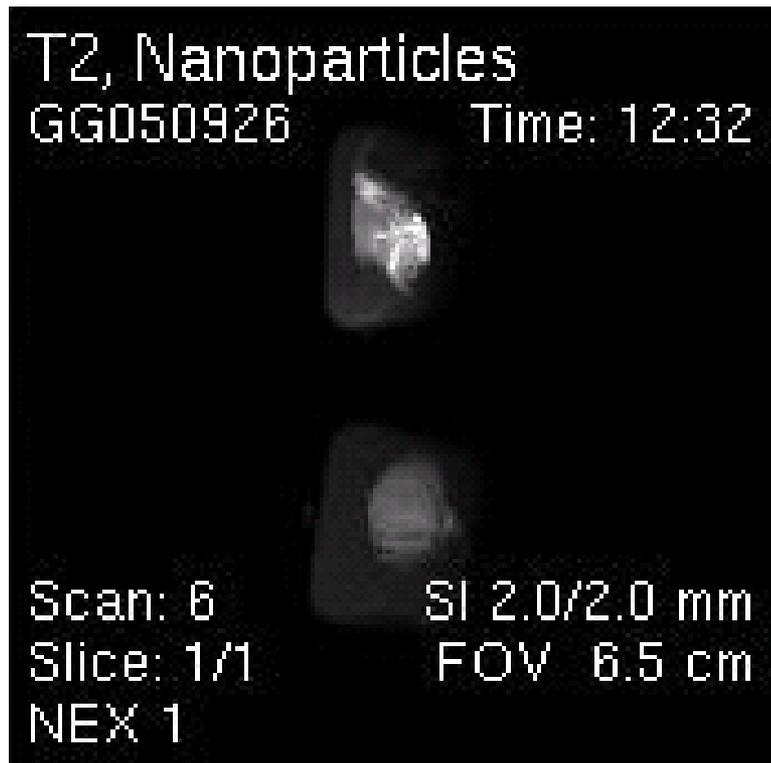
Initial MRI Experiments: Cherry Tomato and Grape

- Injected grapes with saturated saline solution of nanoparticles
- Observed contrast at the location of the injection (nanoparticles)

The iron creates a magnetic field in the water, thus creating a blind spot (dark) for the MRI



T2 Images of Tumors – Contrast Enhancement Due to LHRH-MNPs



Summary and Concluding Remarks

- Overview of some recent work on bioMEMS and bio-nanotechnology for disease (mostly cancer) detection and treatment
- Nanoscale biocompatible titanium coatings and micro-grooves promote adhesion and contact guidance on bioMEMS surfaces
- In-vitro and in-vivo TEM reveal stages of specific nanoparticle attachment and encryption
- LHRH-coated magnetite particles provide opportunities for early MRI detection and treatment of breast & prostate cancer
- PNIPA- Fe_3O_4 systems can be used for hyperthermia and controlled drug release (temperature controlled by MNP concentration and H)